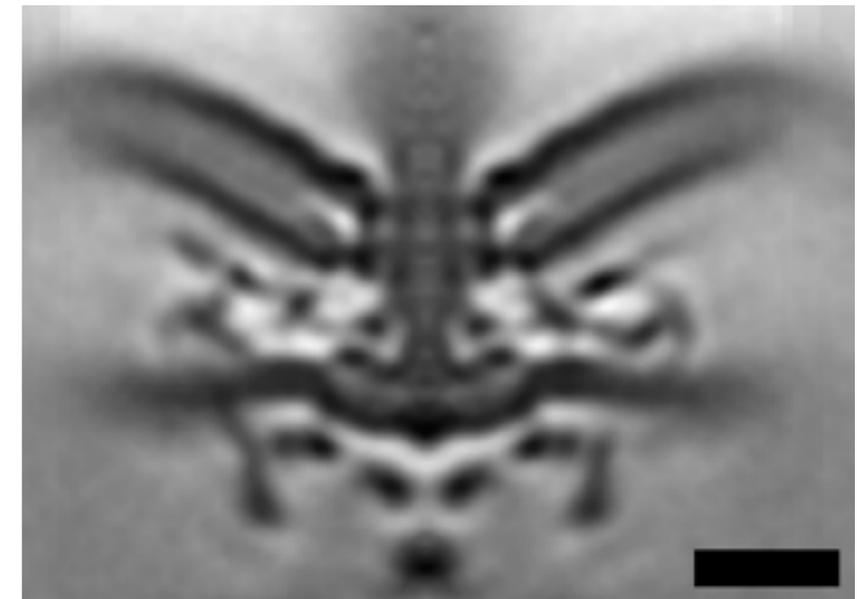
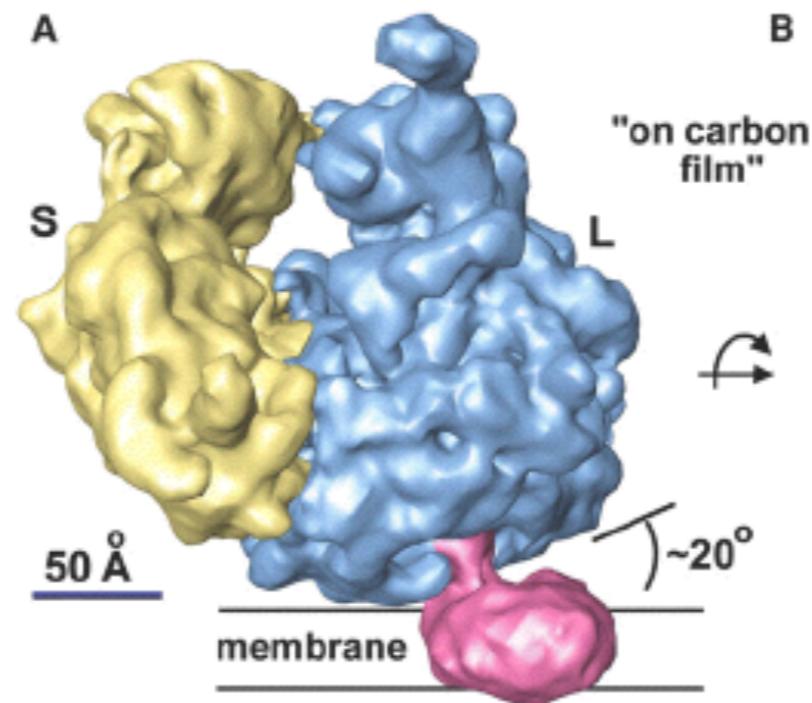
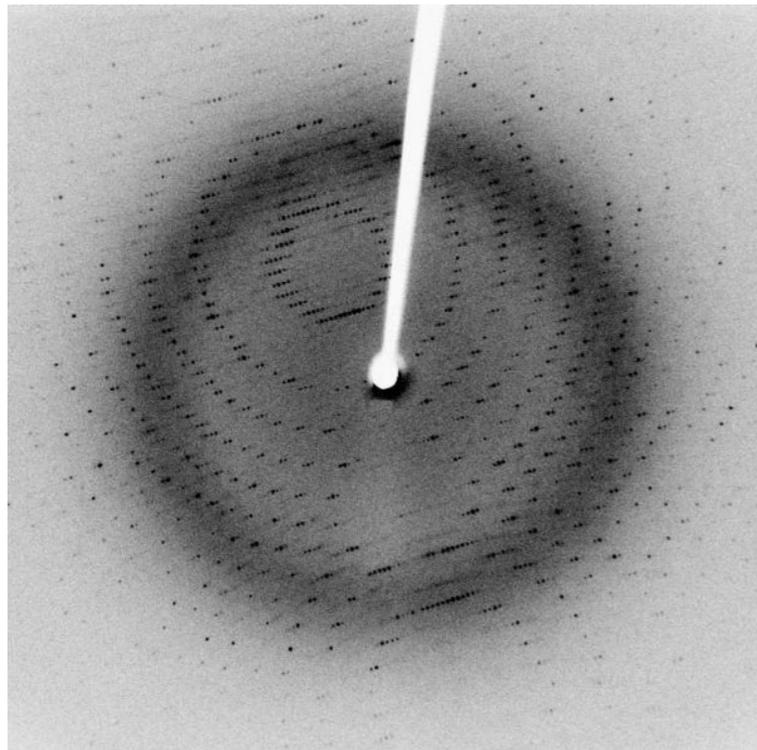


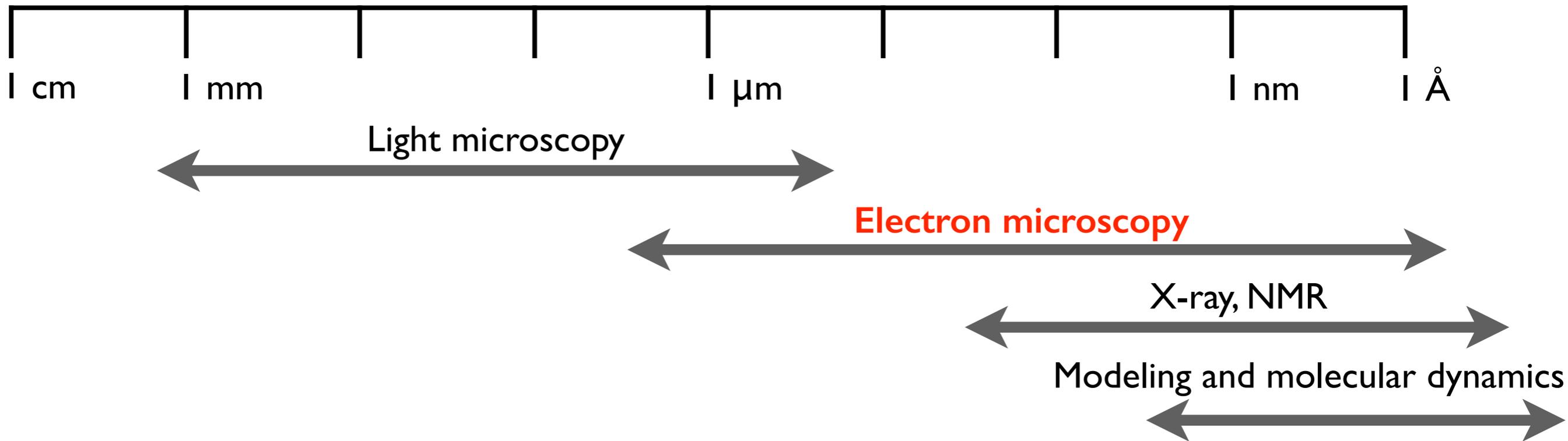
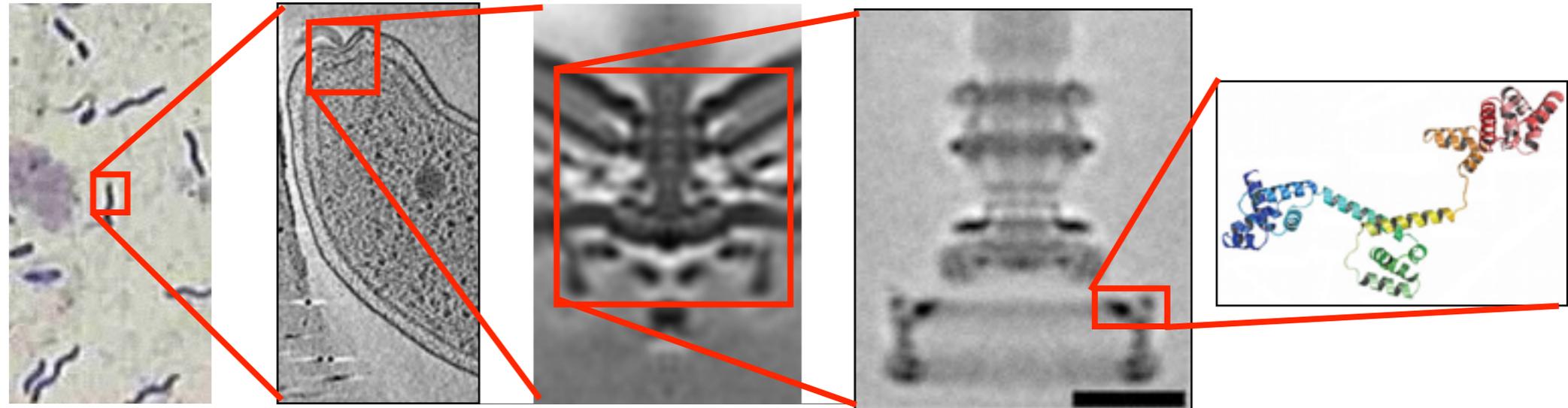
Introduction to structural biology techniques



James C. Gumbart

Georgia Institute of Technology

Structural biology continuum



resolution of the resulting image is limited by the wavelength of light used

$$d = \frac{\lambda}{2(n \sin \theta)}$$

Abbe diffraction limit

Four radiation types

	Advantages	Disadvantages
<i>Visible light</i>	Low sample damage Easily focused Visible by eye	Long wavelengths
<i>X-rays</i>	Small wavelength (Angstroms) Good penetration	Hard to focus Damage sample
<i>Electrons</i>	Small wavelength (pm!) Can be focused	Poor penetration Damage sample
<i>Neutrons</i>	Low sample damage Small wavelength (pm)	How to produce? How to focus?

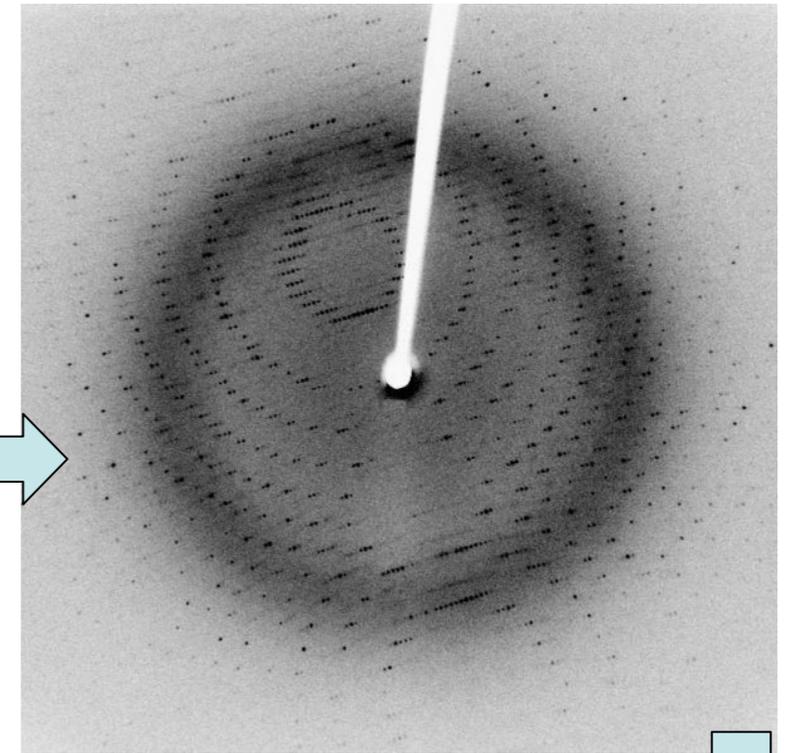
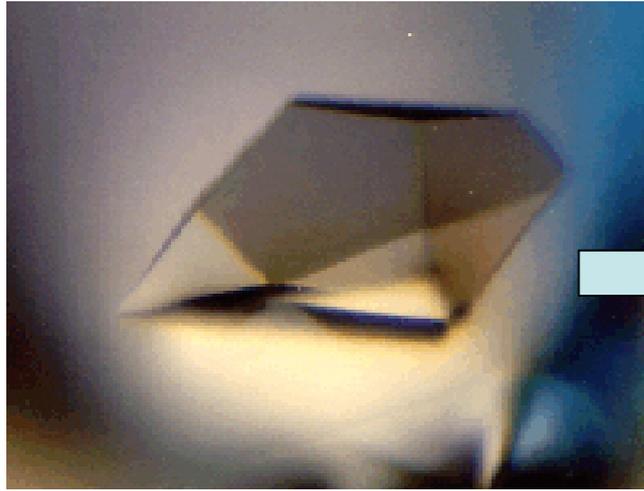


de Broglie, defends thesis in 1924, wins Nobel Prize in 1929

de Broglie wavelength: $\lambda = \frac{h}{p}$

10 keV electron \rightarrow 0.01 nm wavelength

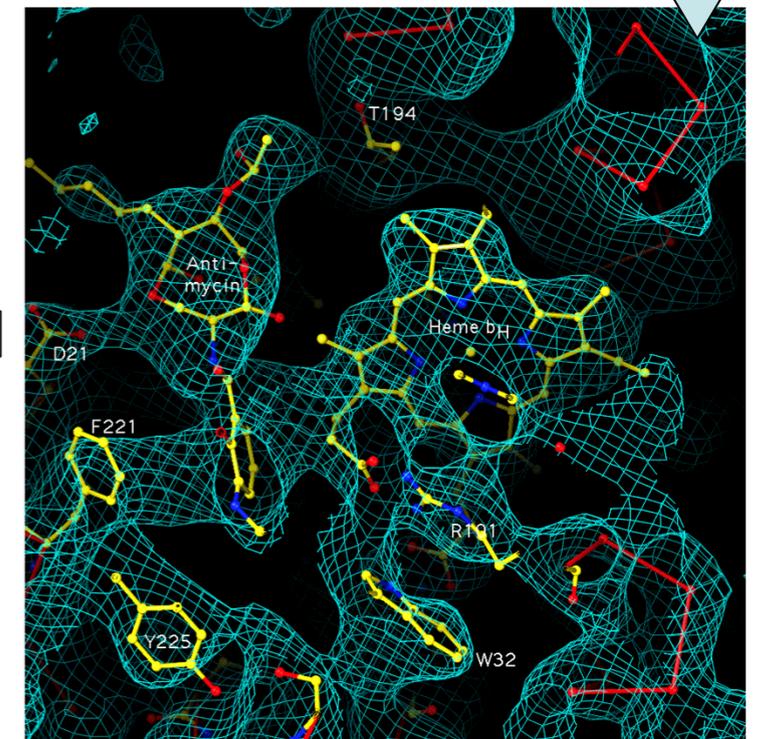
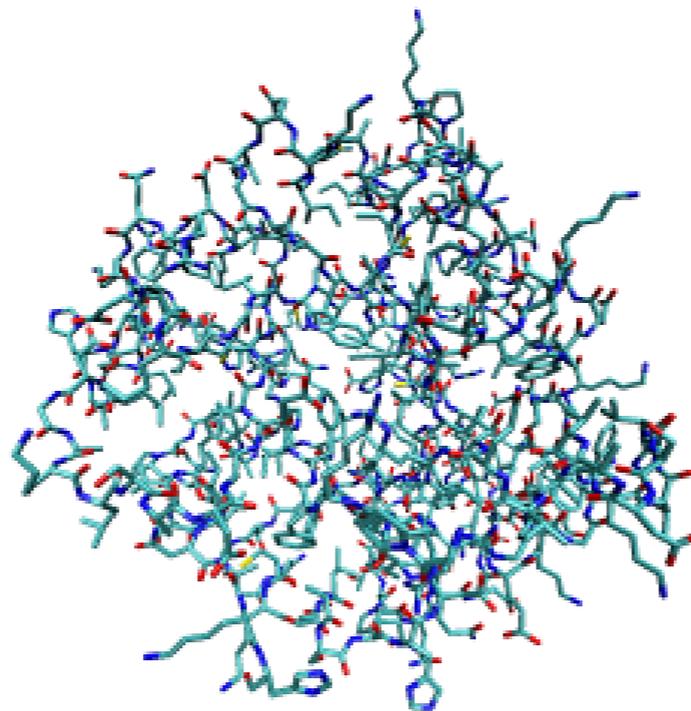
X-ray crystallography



best resolution produced by X-rays, which have wavelengths on the scale of Ångstroms

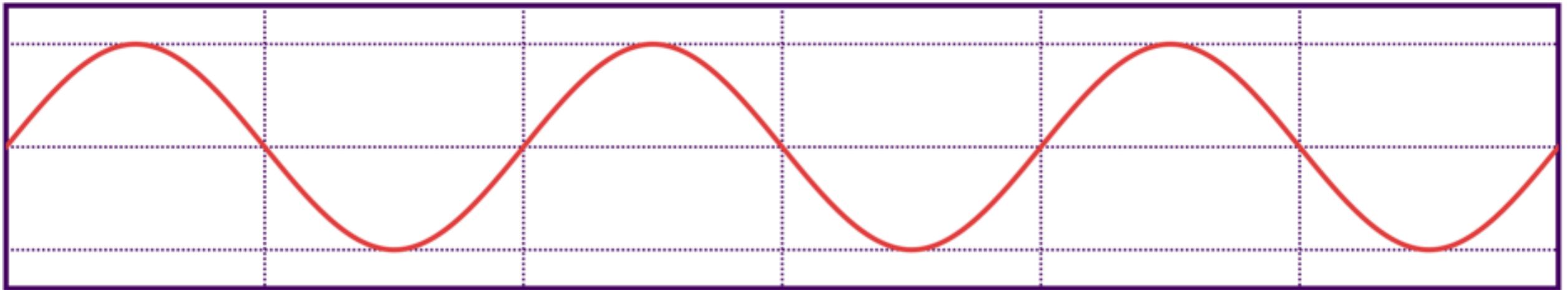
(inverse) Fourier transform

$$f(\mathbf{r}) = \int \frac{d\mathbf{q}}{(2\pi)^3} F(\mathbf{q}) e^{i\mathbf{q}\cdot\mathbf{r}}$$



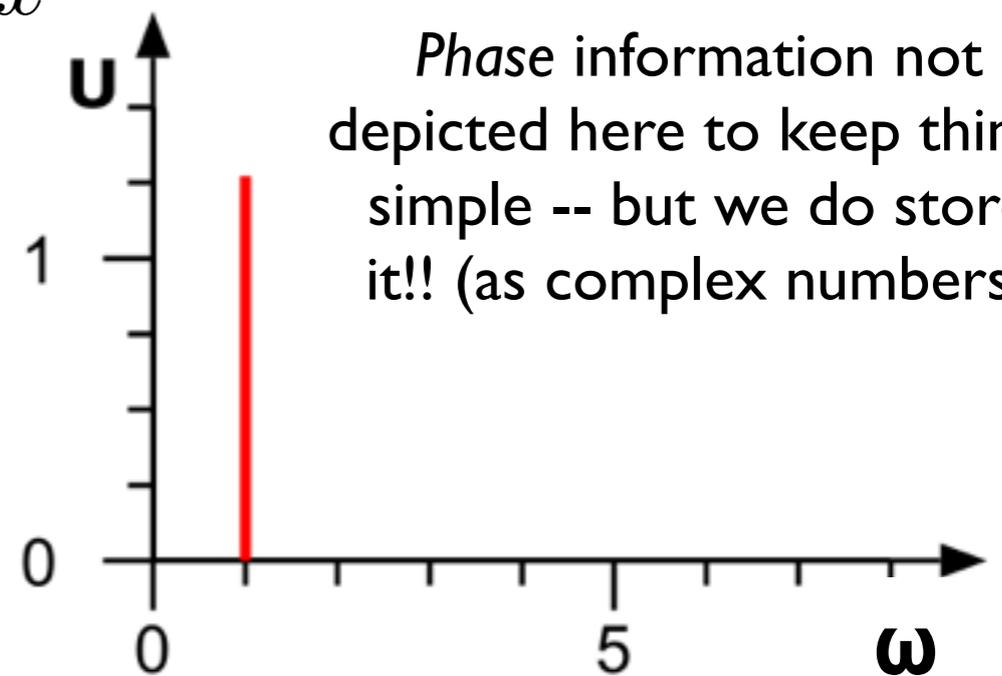
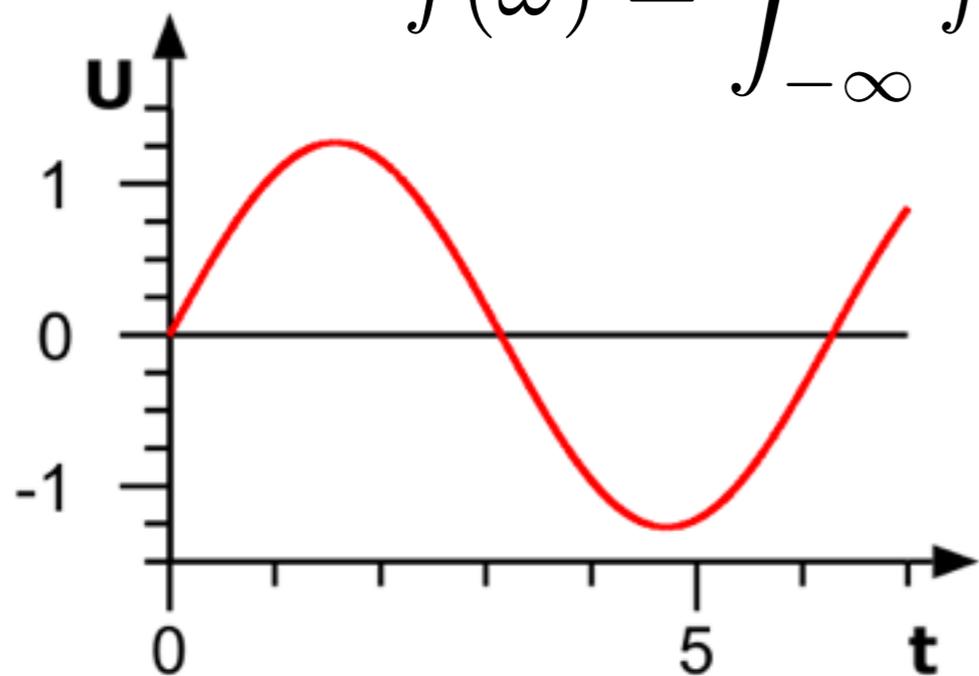
Fourier transforms

properties defining a sine wave:
amplitude, wavelength (or frequency), phase shift, and direction



Waves can be represented in frequency (“*reciprocal*”) space

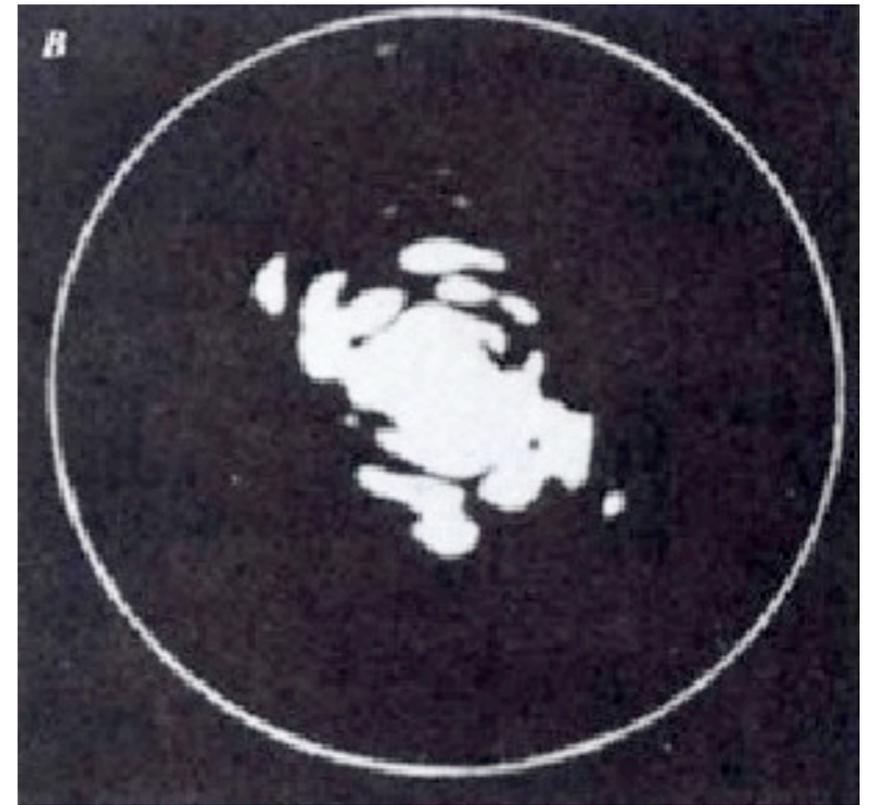
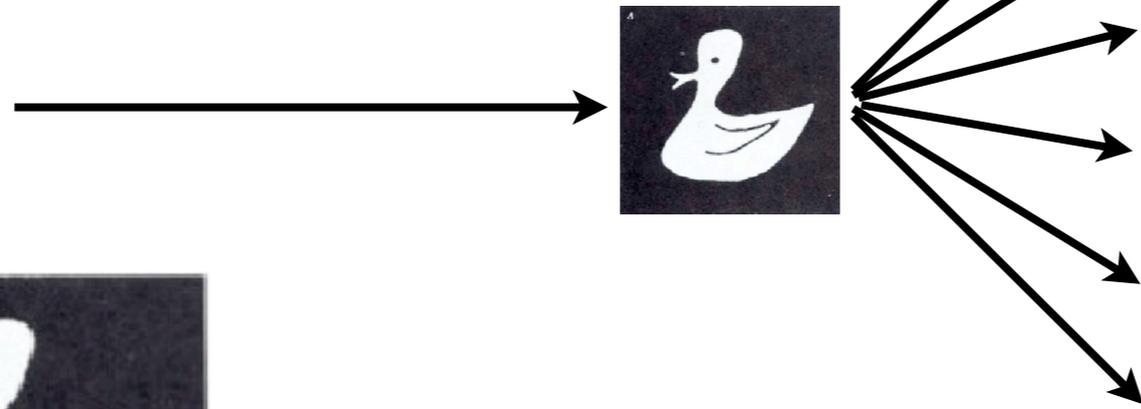
$$\hat{f}(\omega) = \int_{-\infty}^{\infty} f(x) e^{-2\pi i \omega x} dx$$



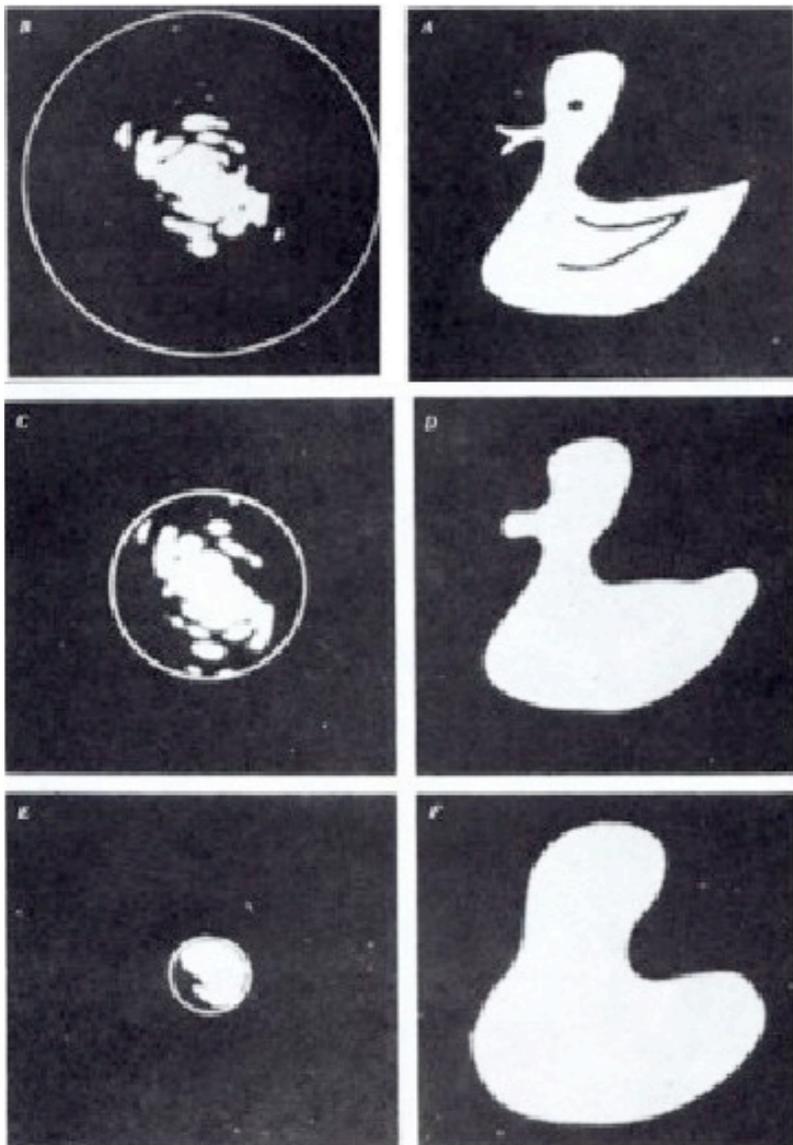
Phase information not depicted here to keep things simple -- but we do store it!! (as complex numbers)

diffraction patterns

diffracted X-rays (or electrons) produce a Fourier transform of the original object



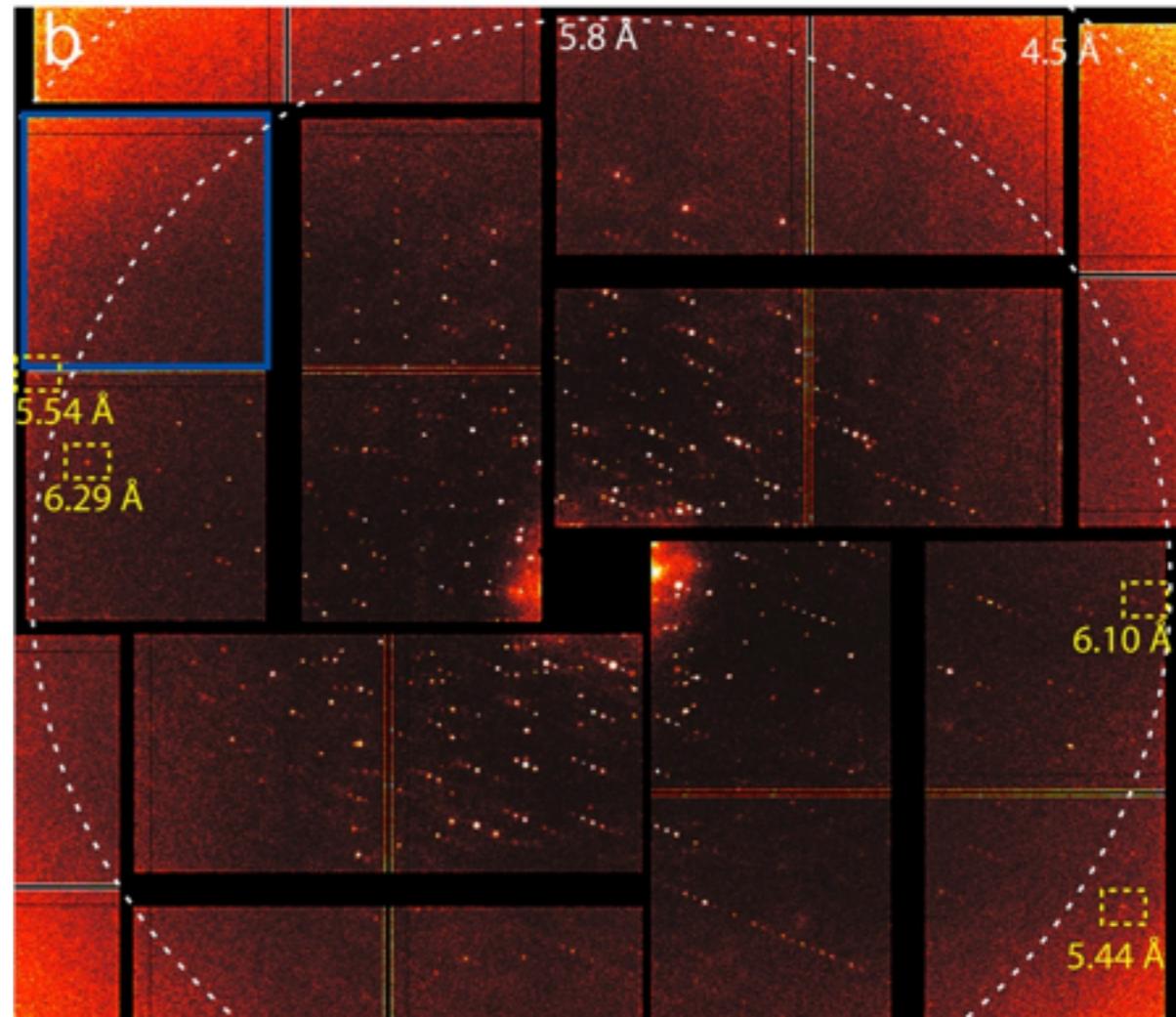
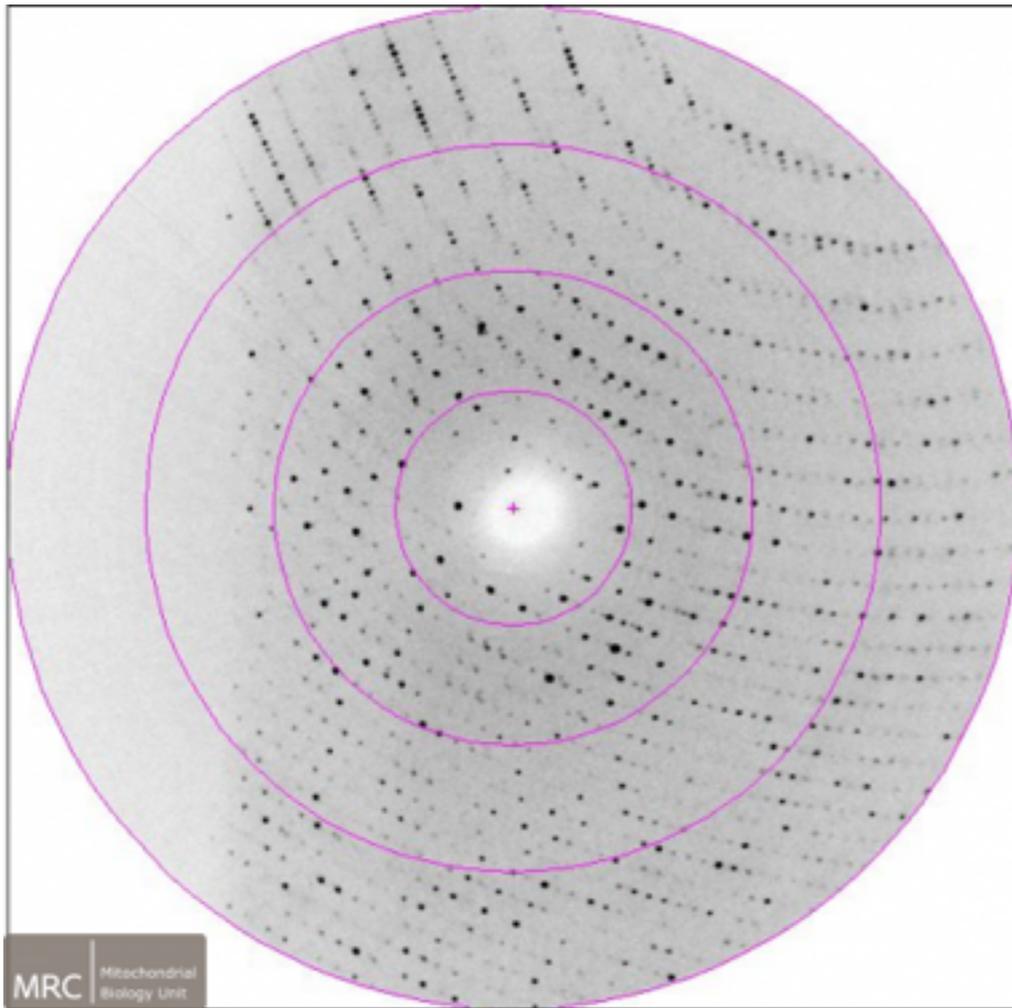
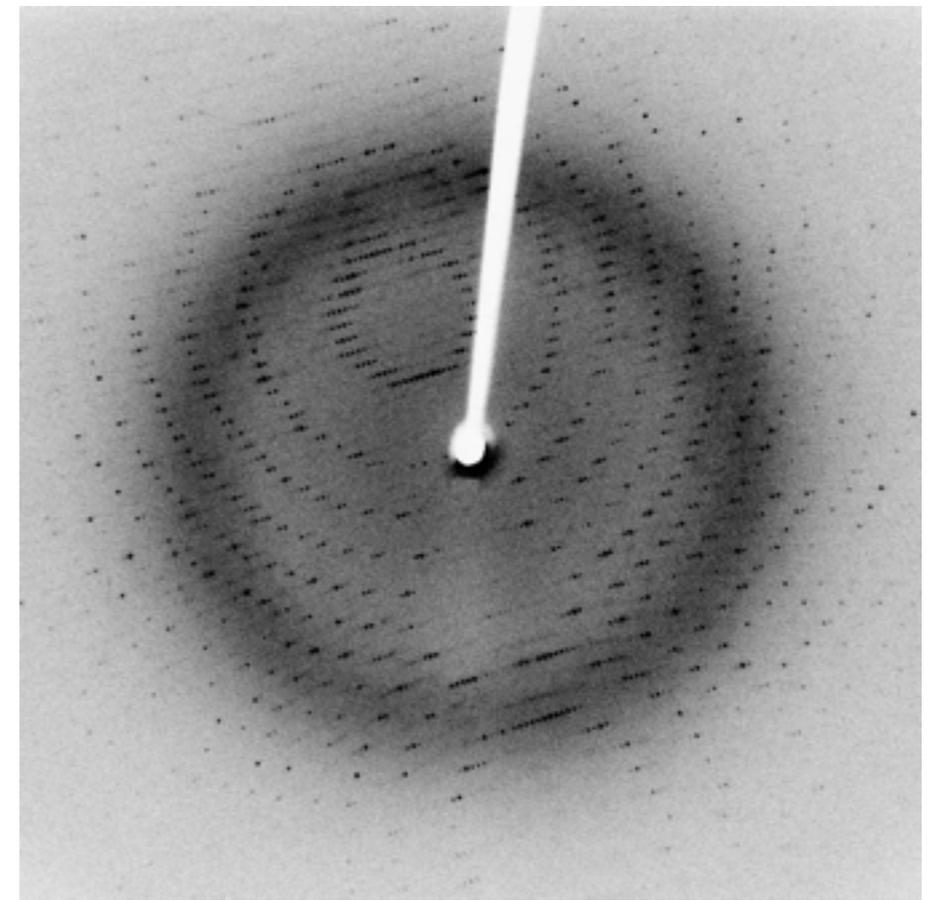
*intensity of diffracted photons
(but not phases!)*



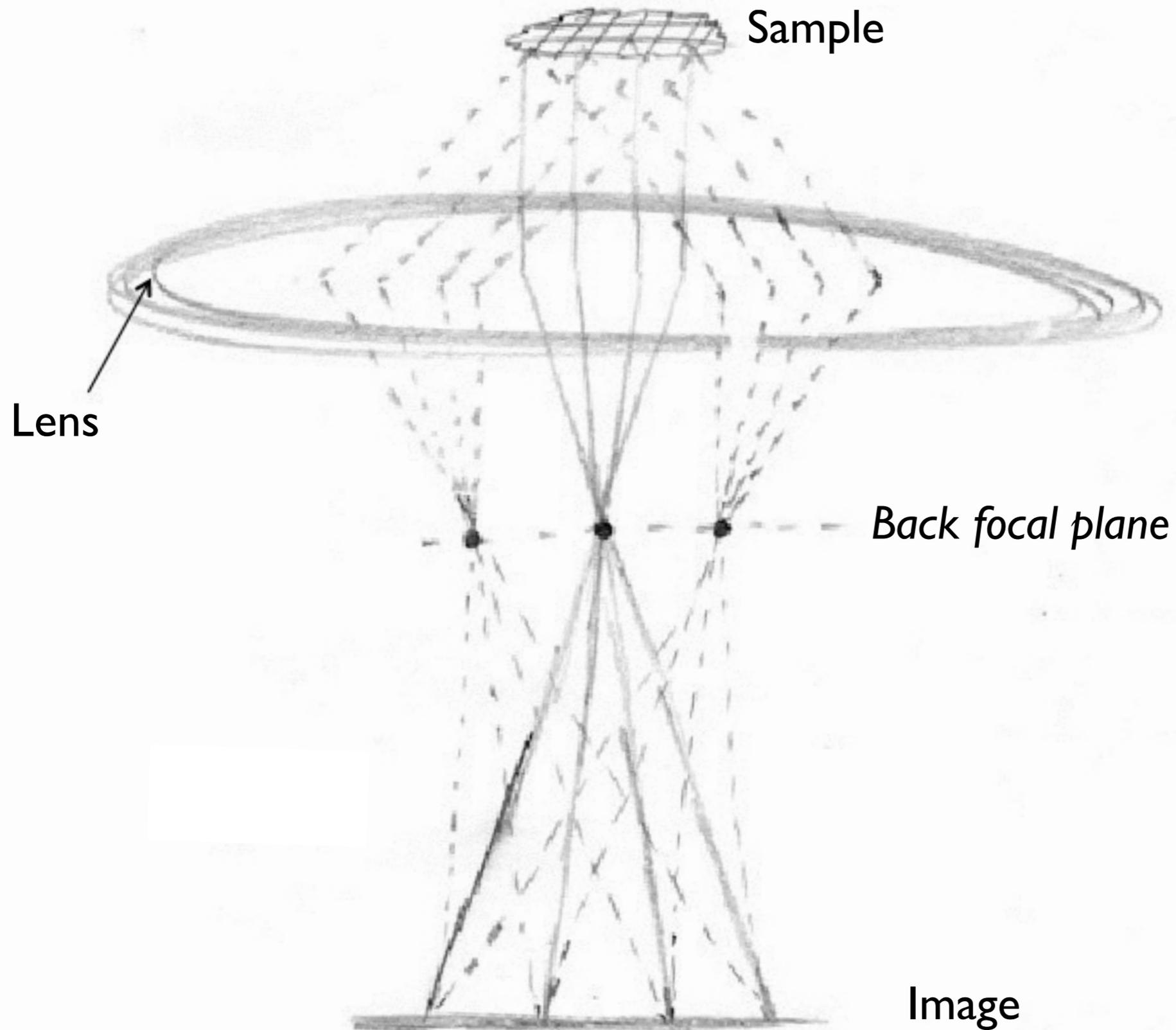
High “frequency” components contribute the details, and appear furthest from the origin

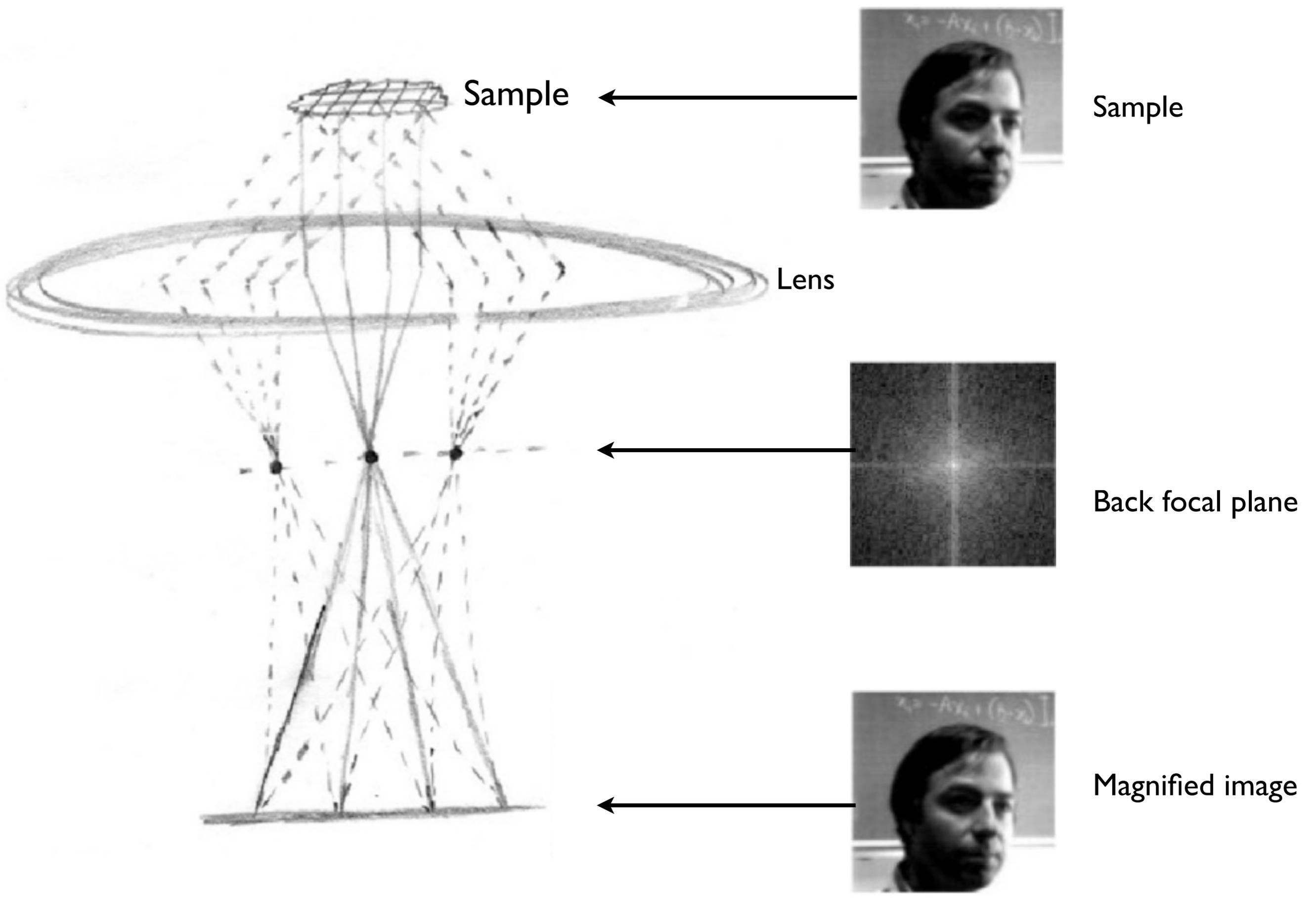
diffraction patterns

resolution determined by presence of data far from origin



Before inverting reciprocal space back into an image, the diffraction pattern (i.e. Fourier transform) is focused at the **back focal plane**:



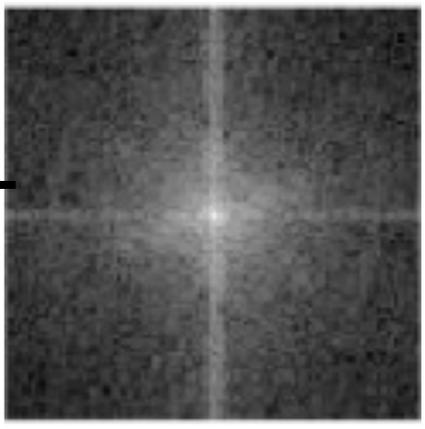


Sample



Sample

Lens



Back focal plane

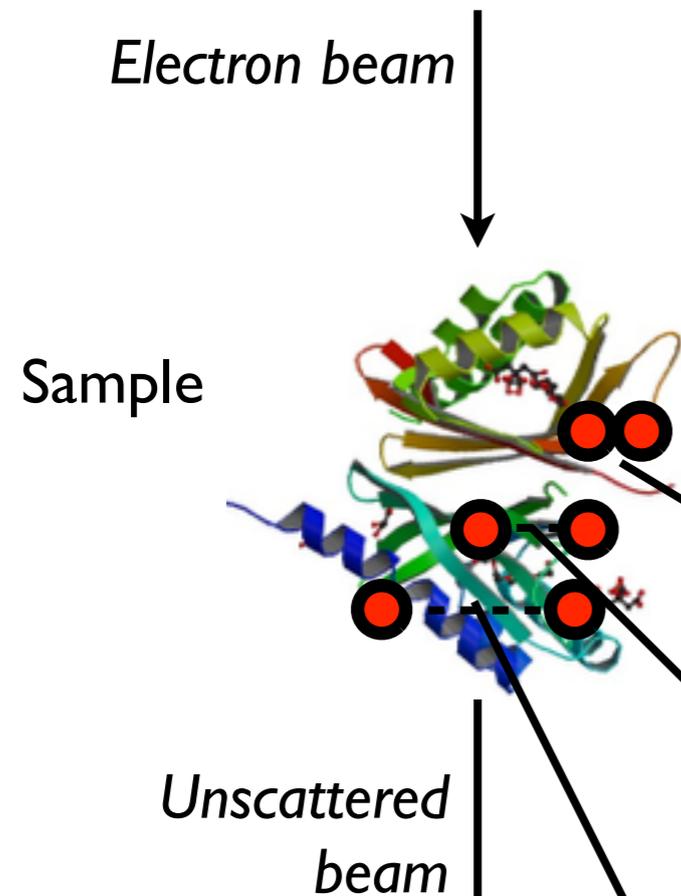


Magnified image

reconstituting the image

normally, use a lens to refocus rays onto the sensor, *but...*

there are no X-ray lenses!!!

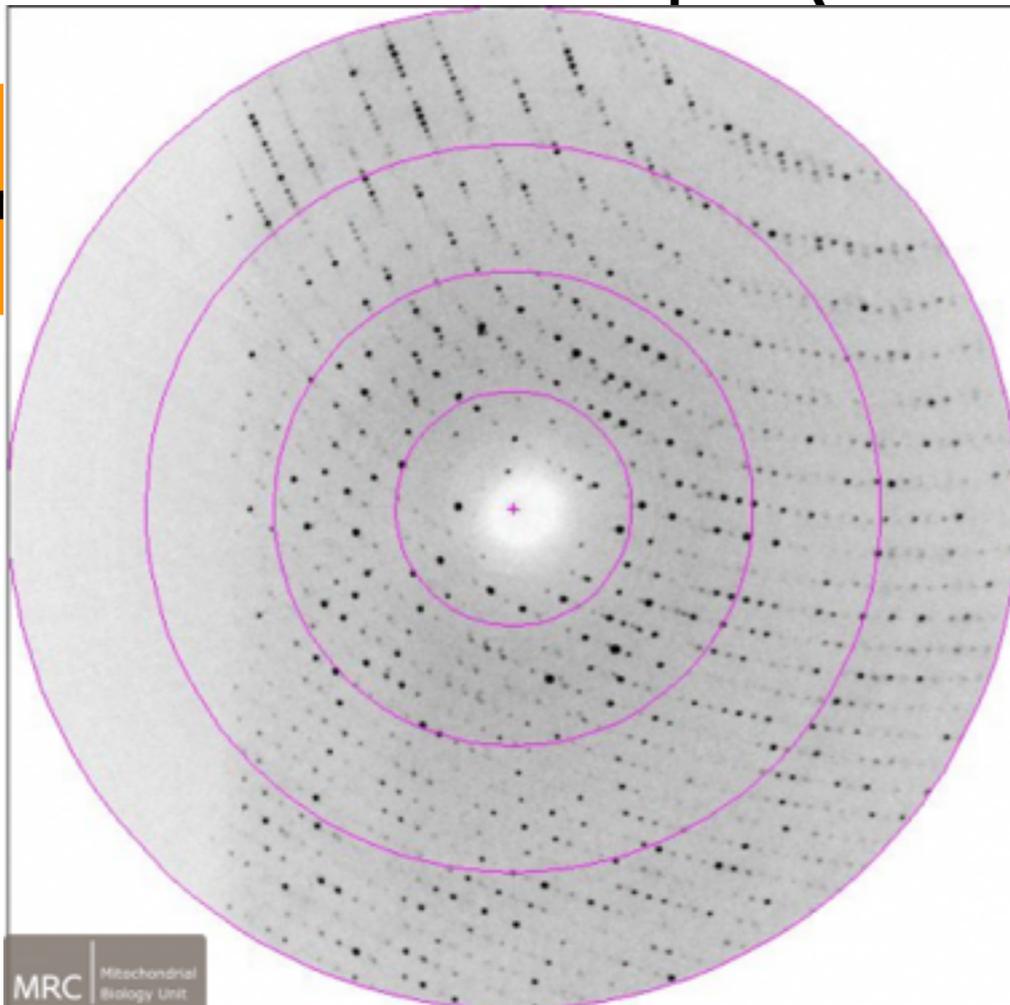


(Low spatial frequency data) ↔ (High spatial frequency data)

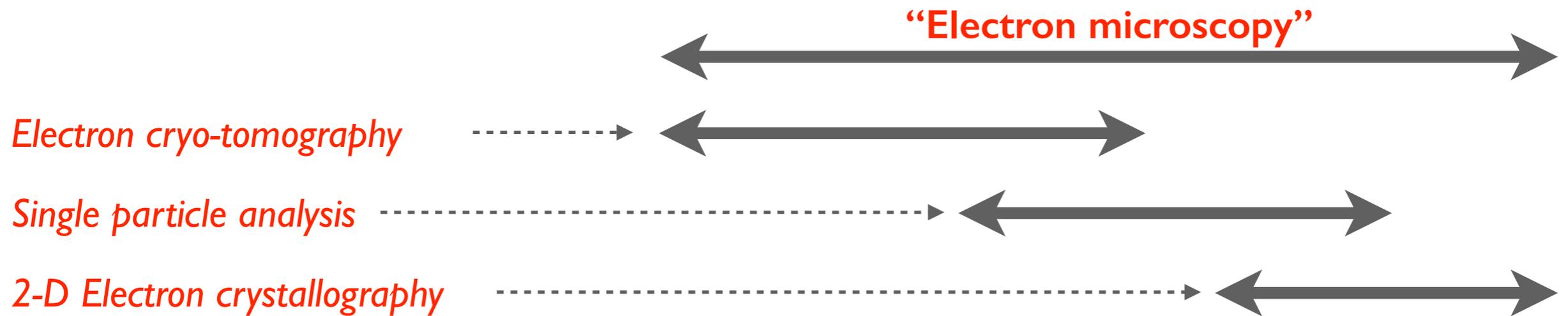
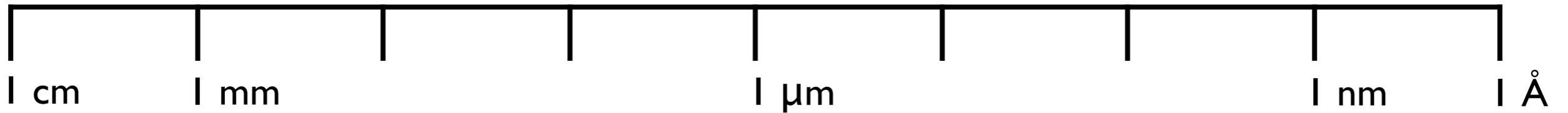
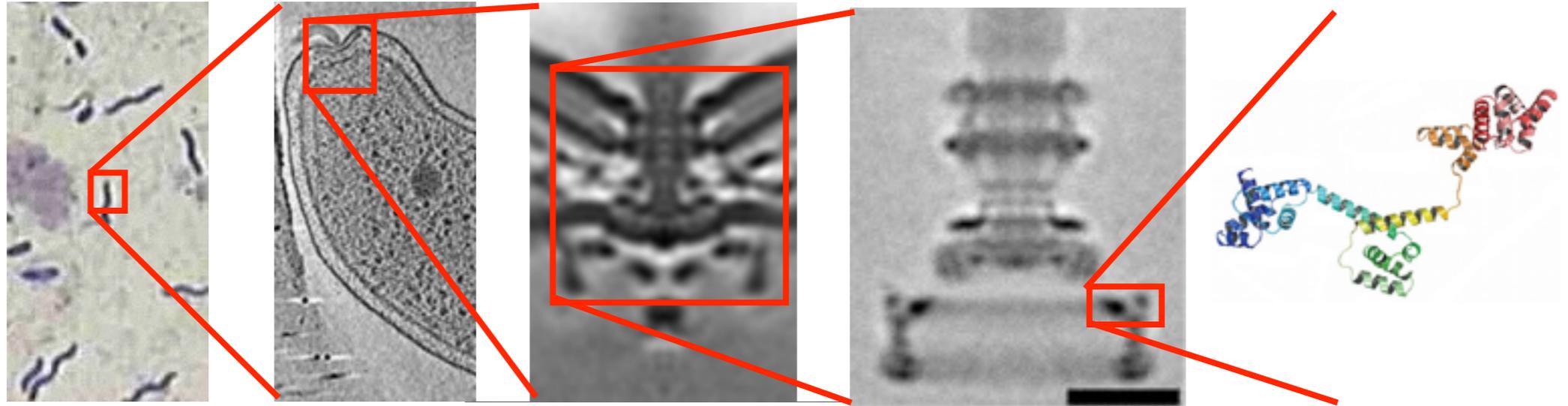
i.e., diffraction = Fourier transform

so we only have the diffraction pattern, which encodes intensities, but not phases

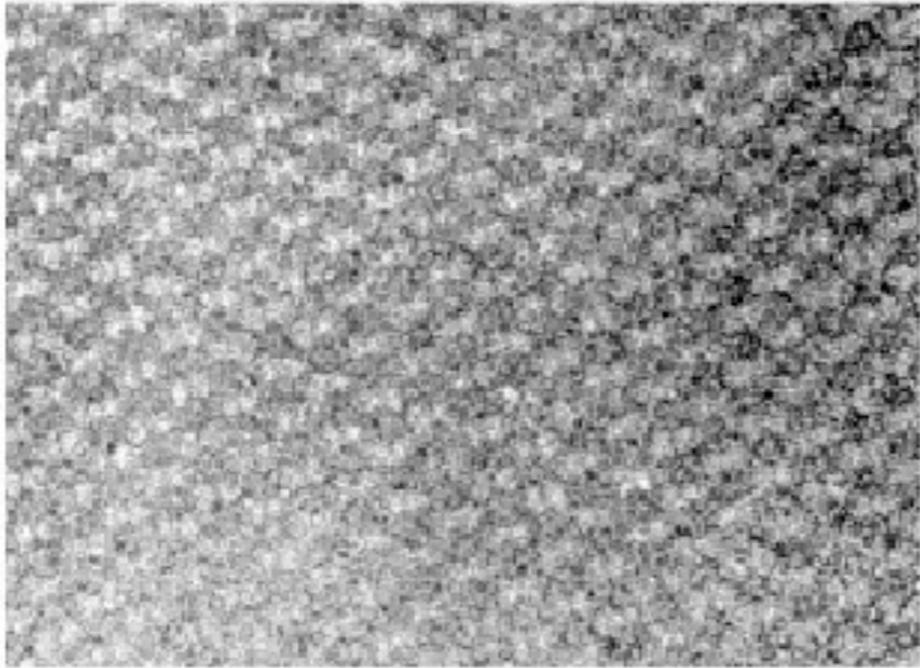
this is the so-called “phase problem”



Structural biology continuum

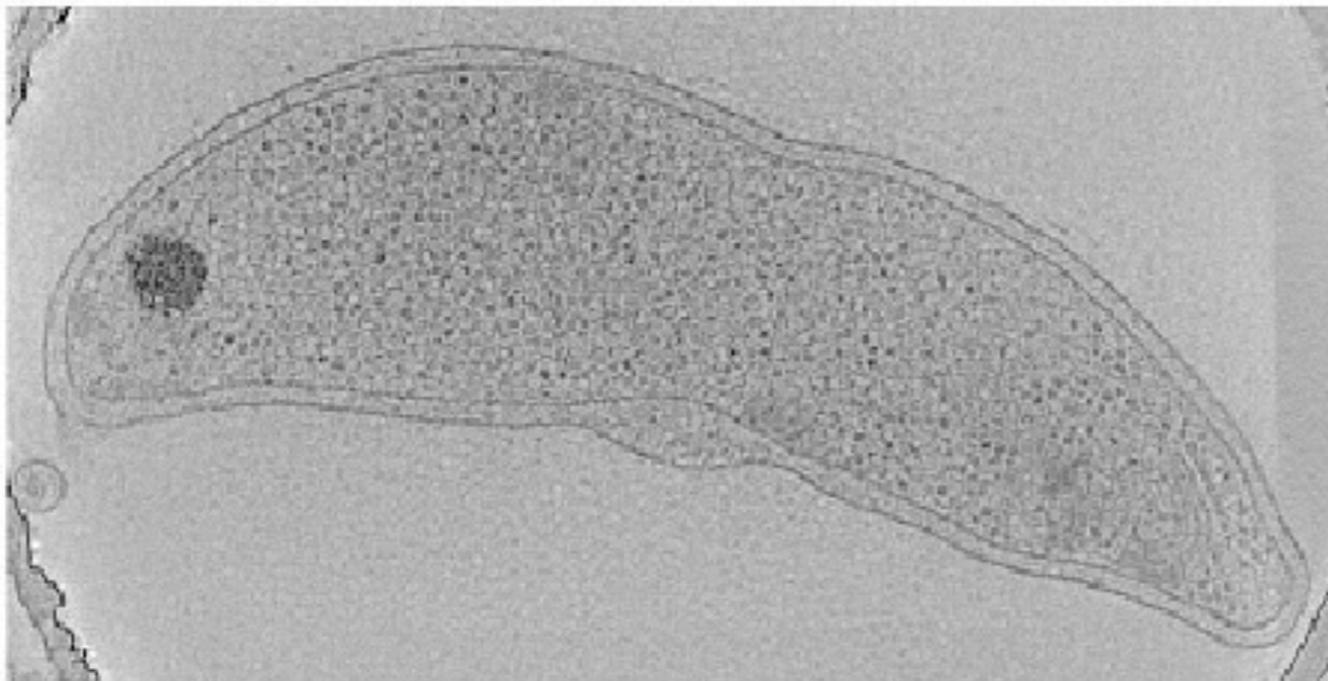


Rough guide to “cryo-EM”:

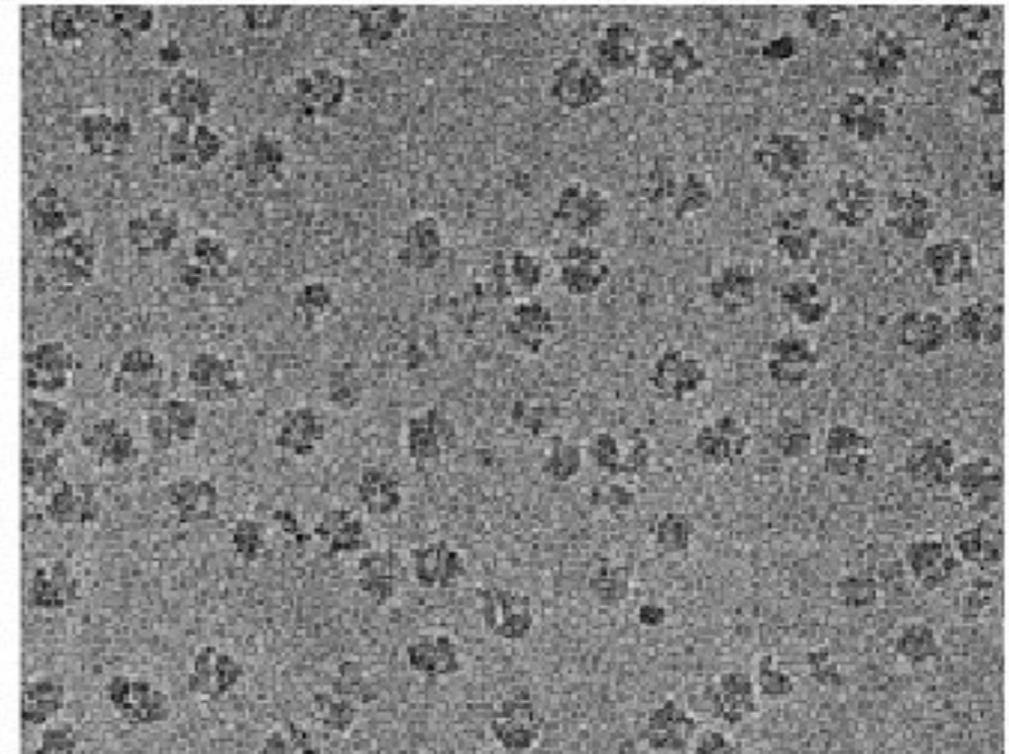


2D electron crystallography

Electron cryo-tomography

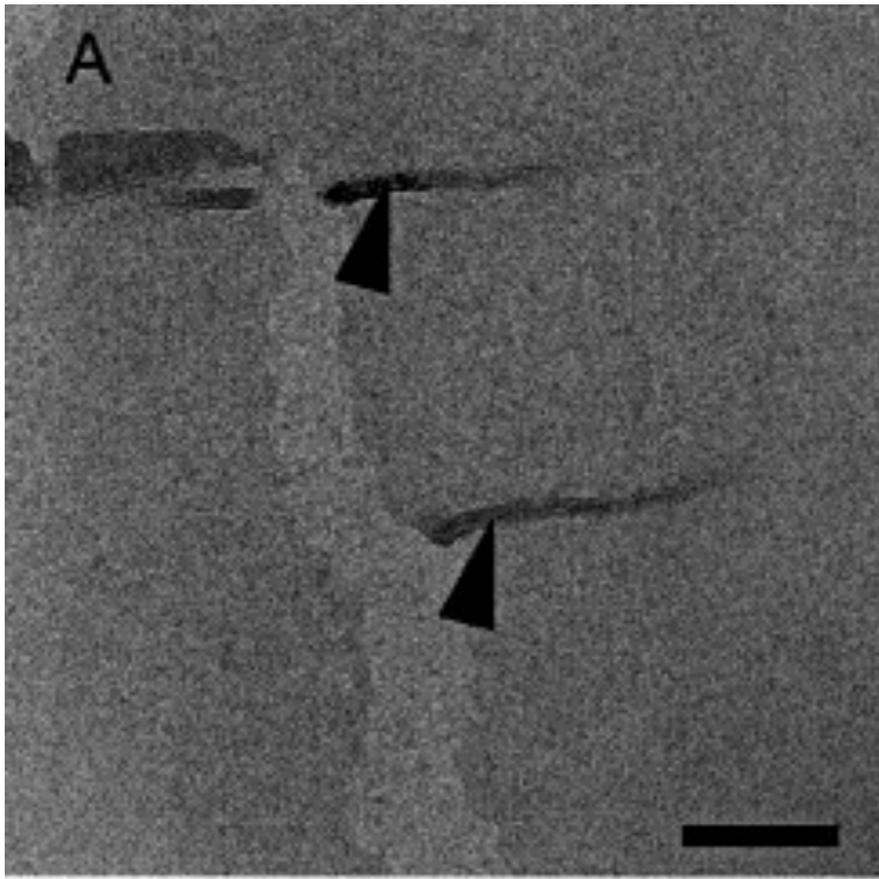


Three flavors:

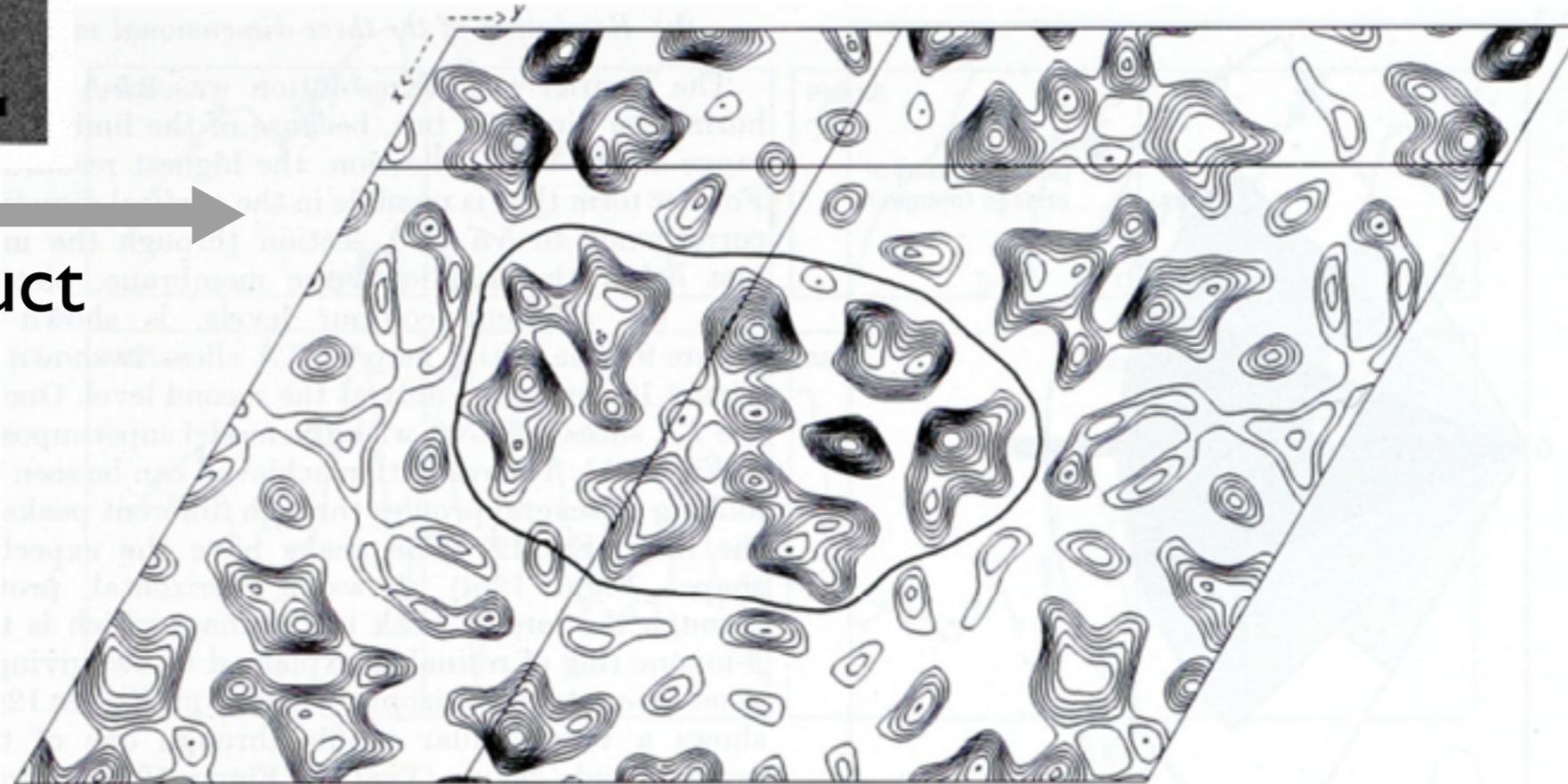


Single particle analysis

2-D electron crystallography



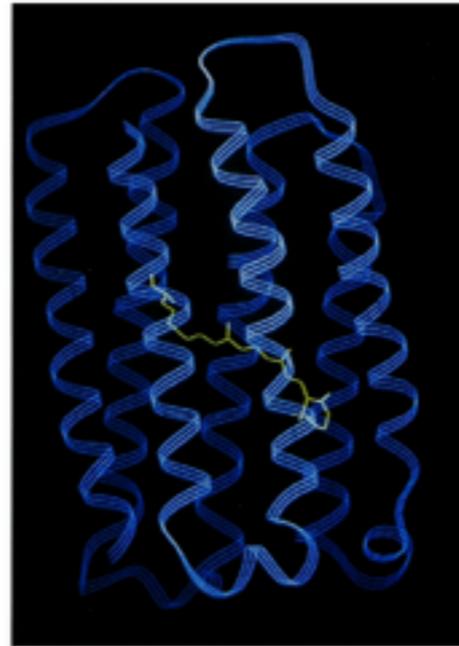
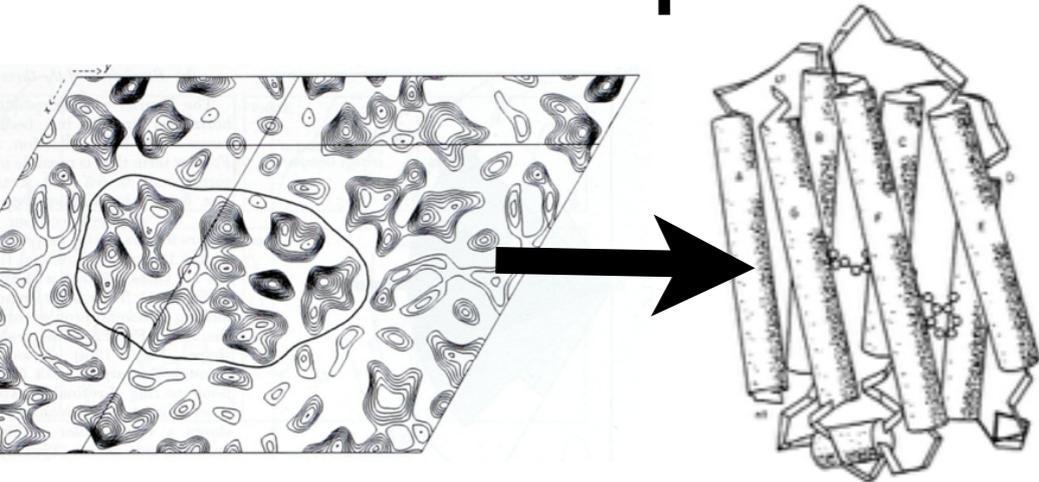
Reconstruct



useful because phases
aren't irretrievably lost
works better with smaller
crystals than X-rays, but
must be thin

Example structures

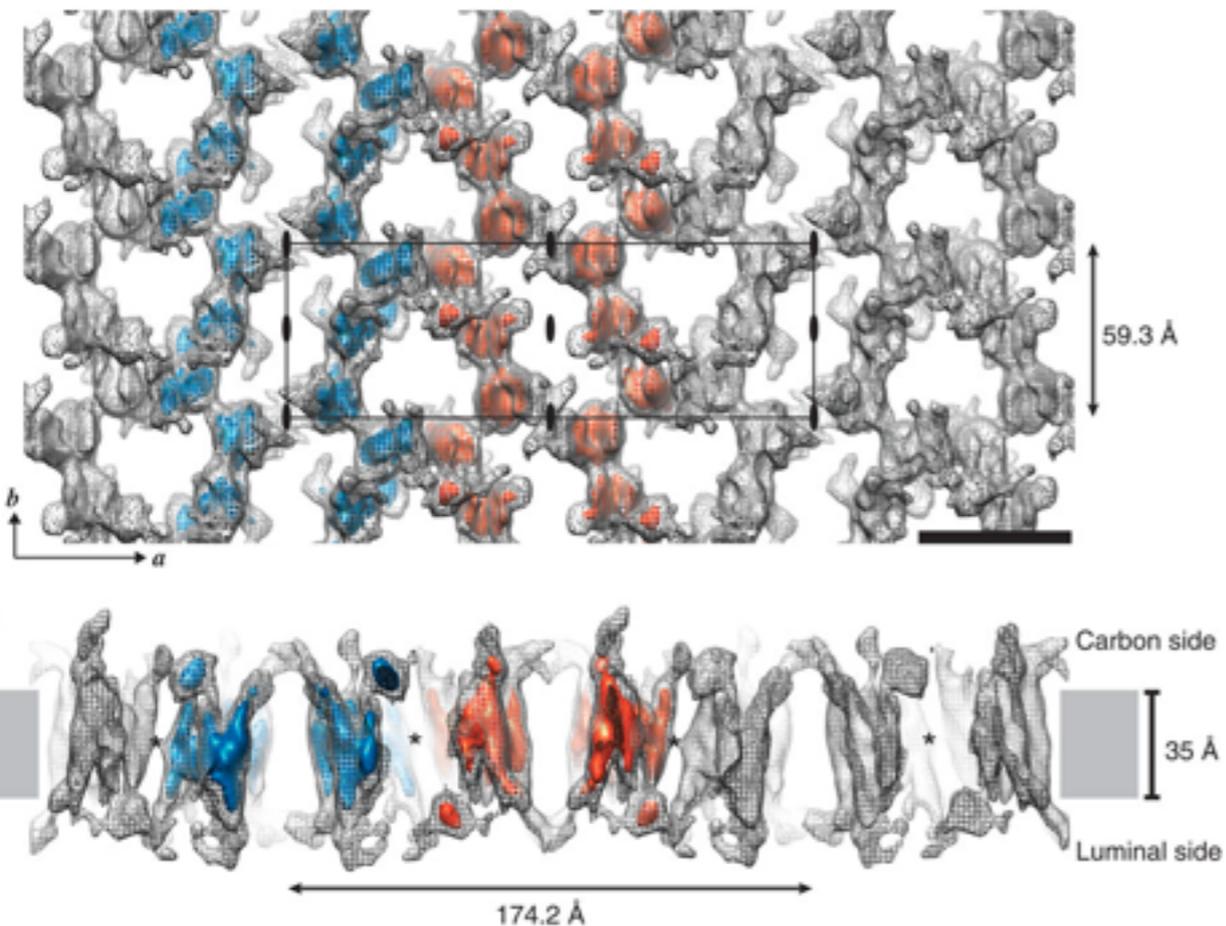
Bacteriorhodopsin



Henderson et al., 1990

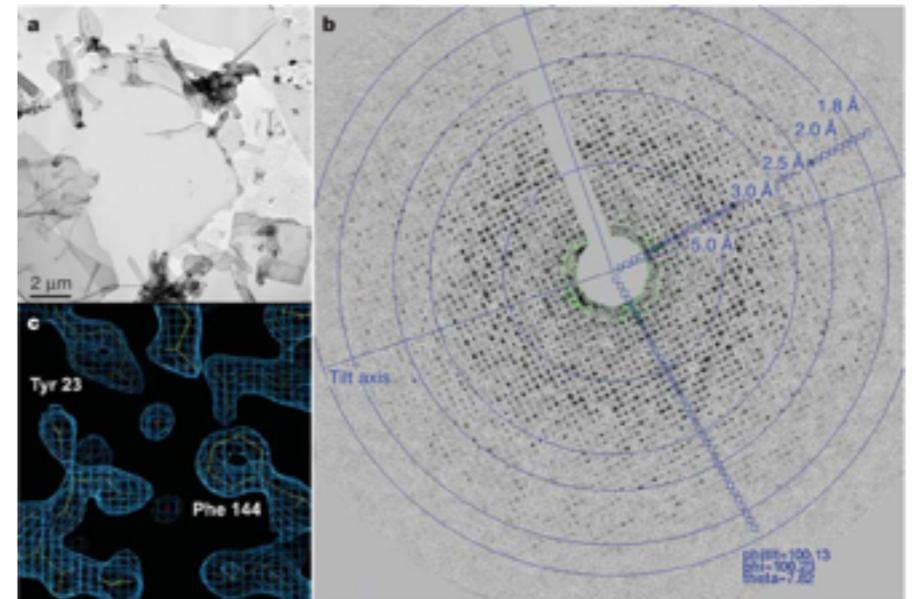
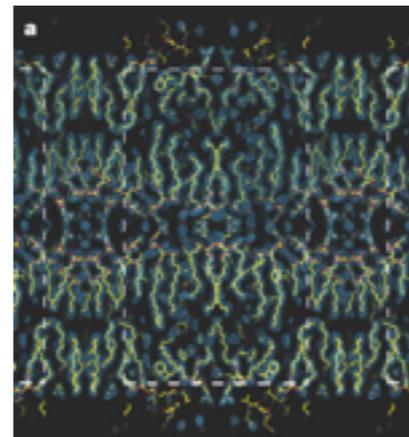
First ever electron crystallography structure, to 3.5 Å.

IP39 (~10Å)



Suzuki et al. (2013) Nat. Comm. 4:1766.

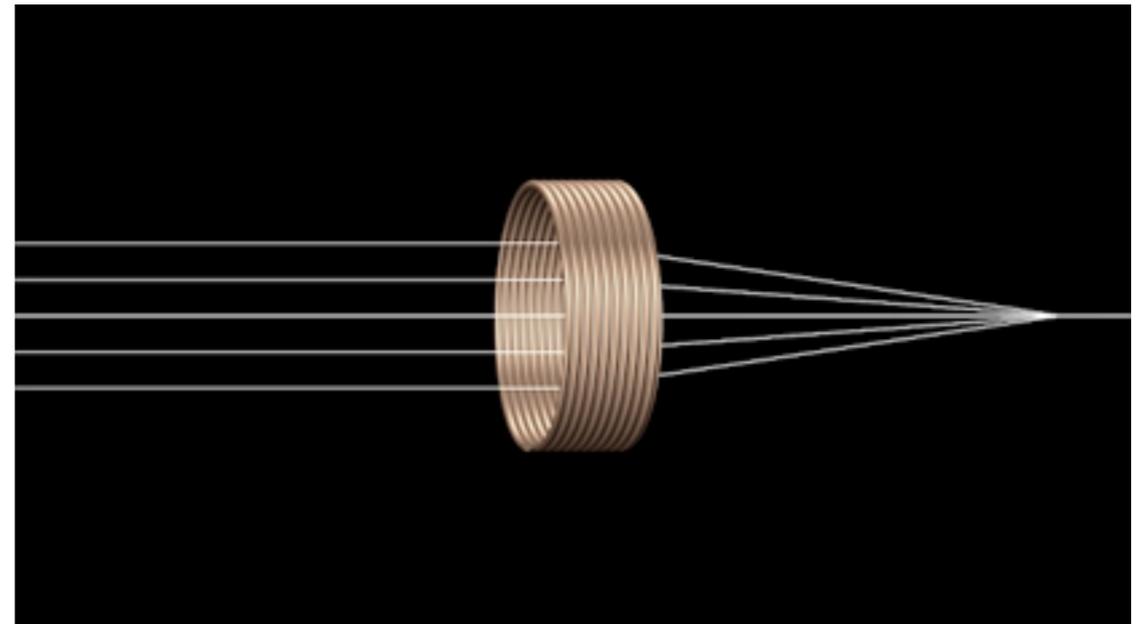
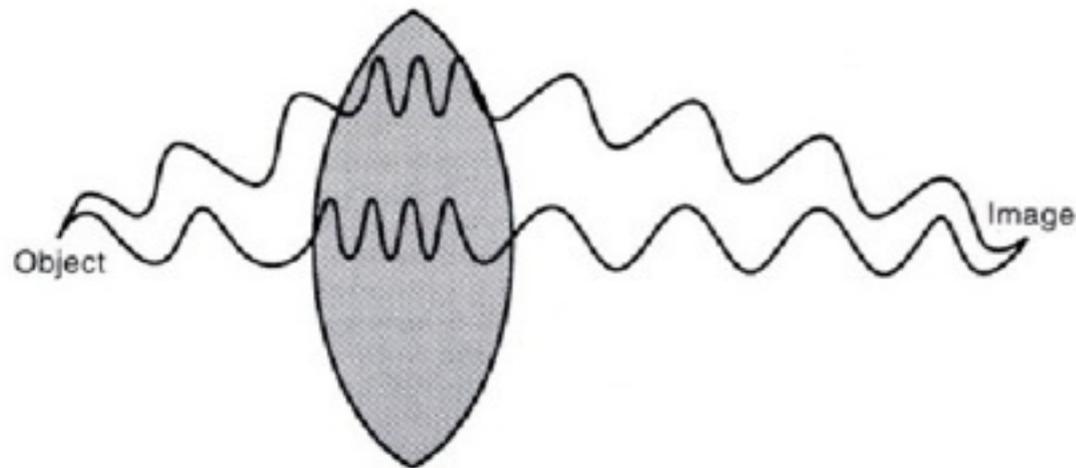
Aquaporin 0 (1.9Å)



Gonen et al., Nature (2005) 438:633

electron lenses

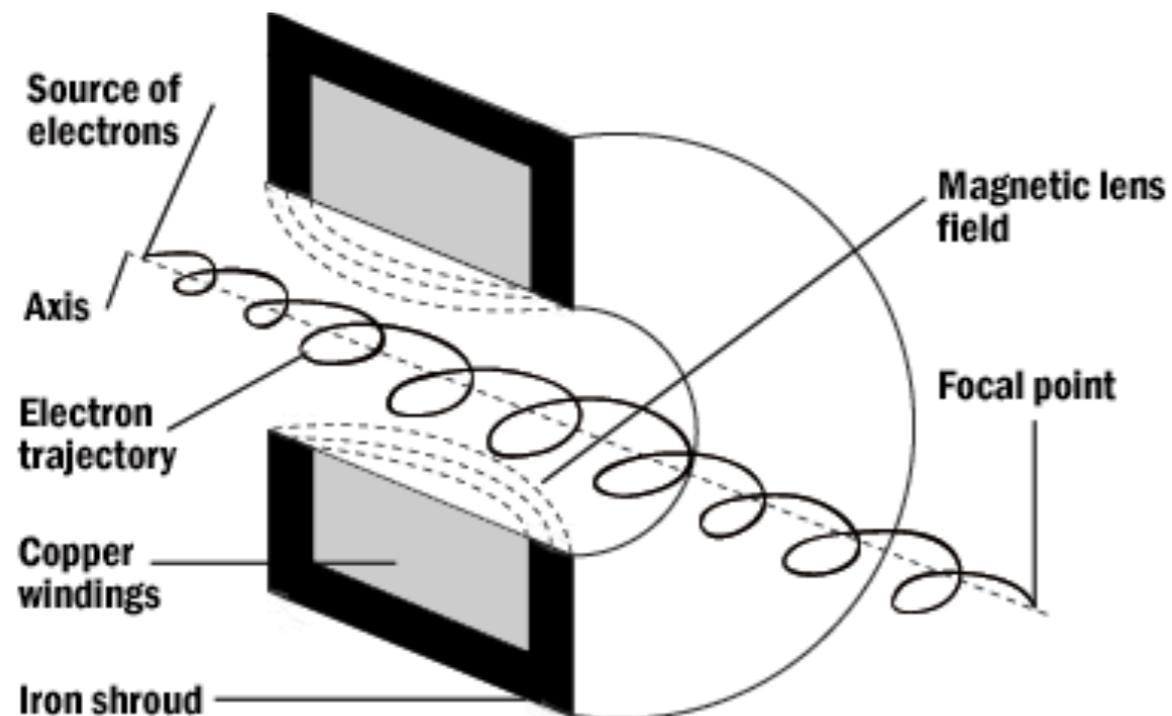
Lenses “focus” divergent (diffracted) rays, allow production of image (including magnification)



<http://www.first-tonomura-pj.net/e/commentary/mechanism/index.html>

For electrons, the “lens” is actually a magnetic field

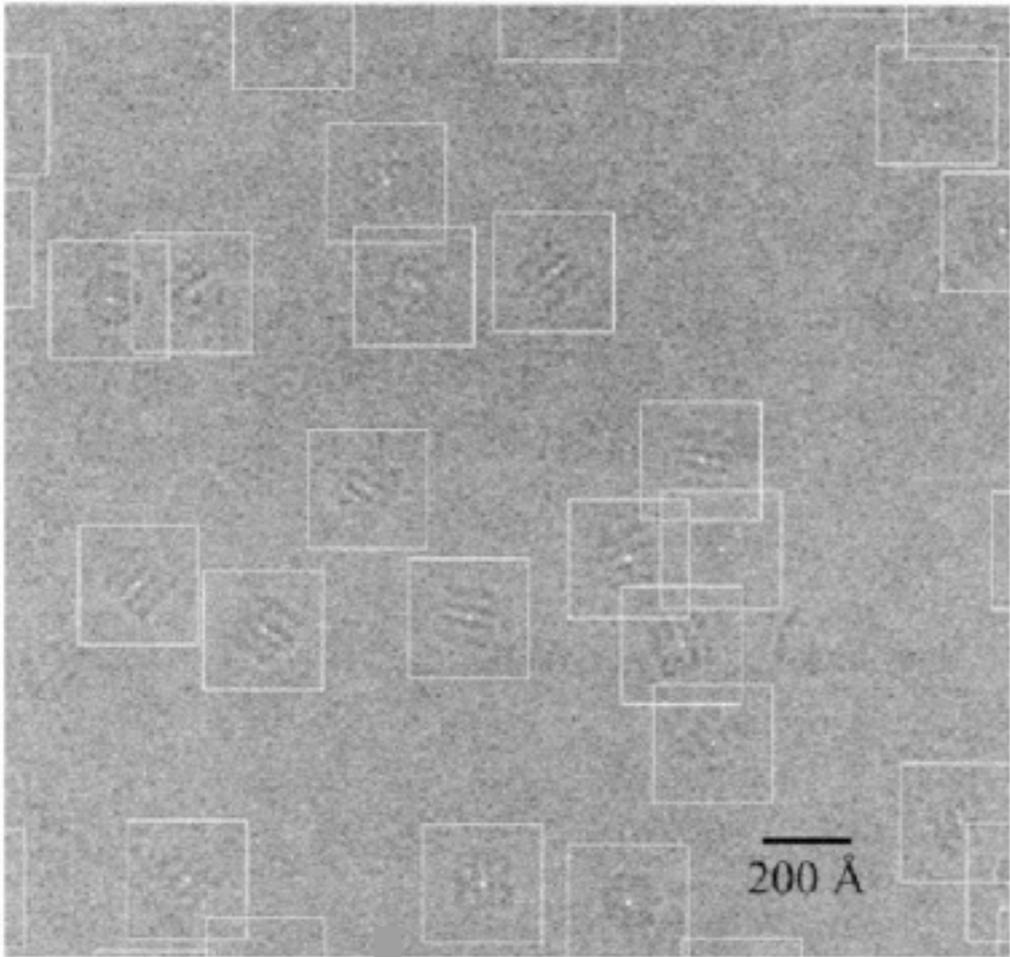
$$\mathbf{F} = -e (\mathbf{v} \times \mathbf{B})$$



spiraling effect required to focus beam, but introduces unavoidable artifacts

Single particle analysis (cryo-EM)

100 000's of ("identical") 2-D particles



Align and average



Initial



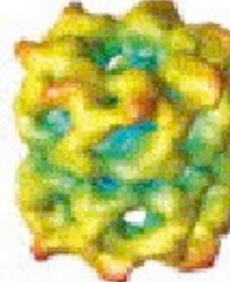
Iter 1



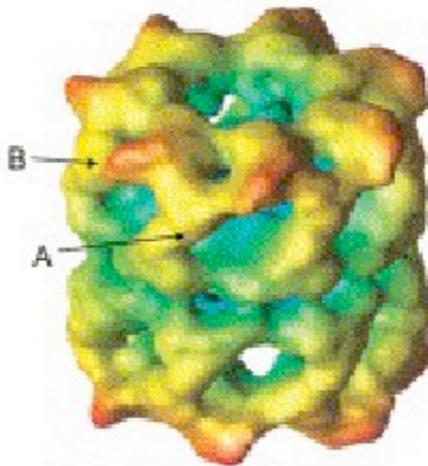
Iter 2



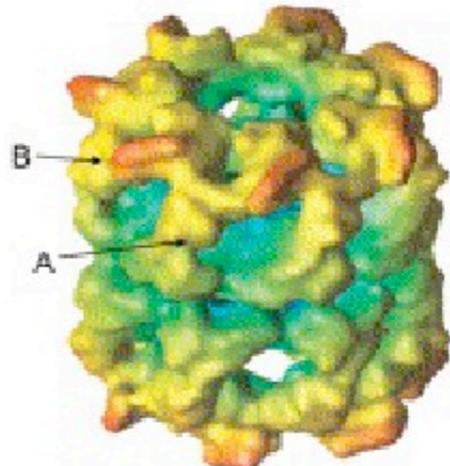
Iter 3



Iter 4

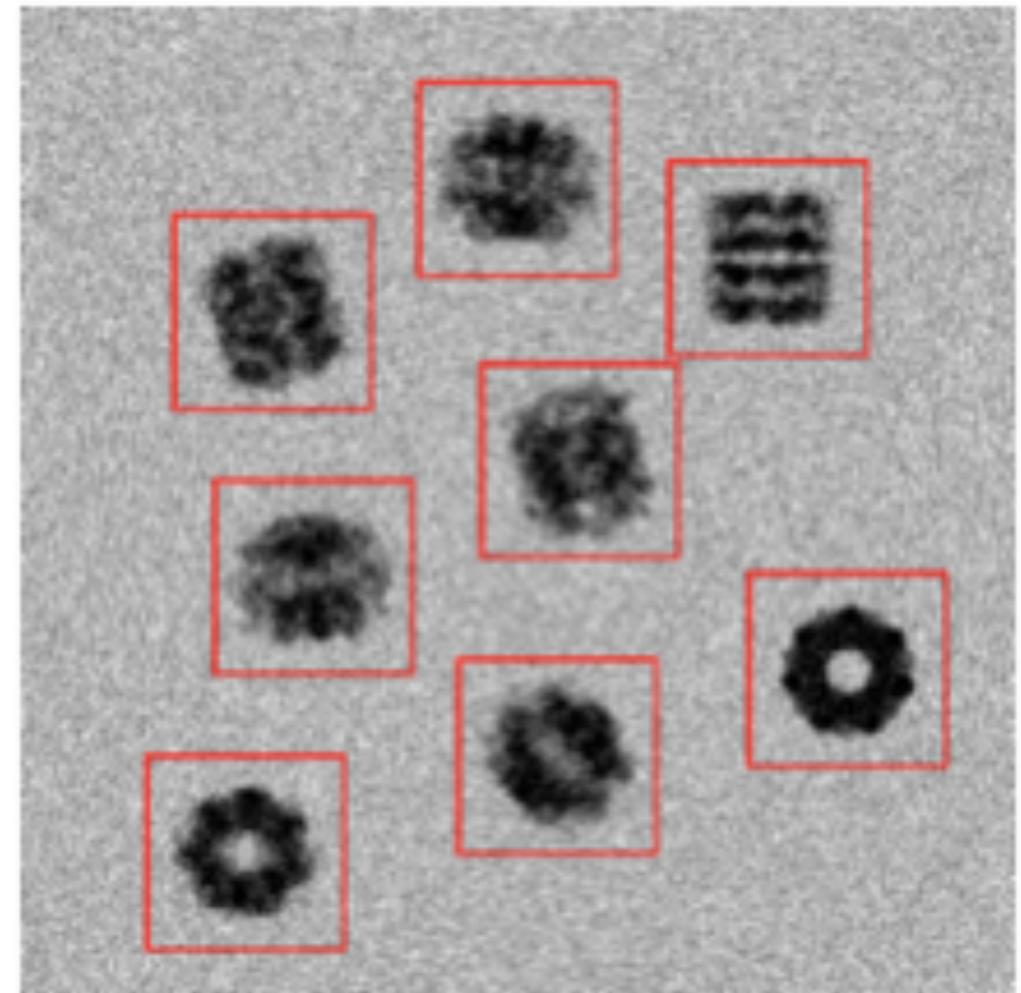
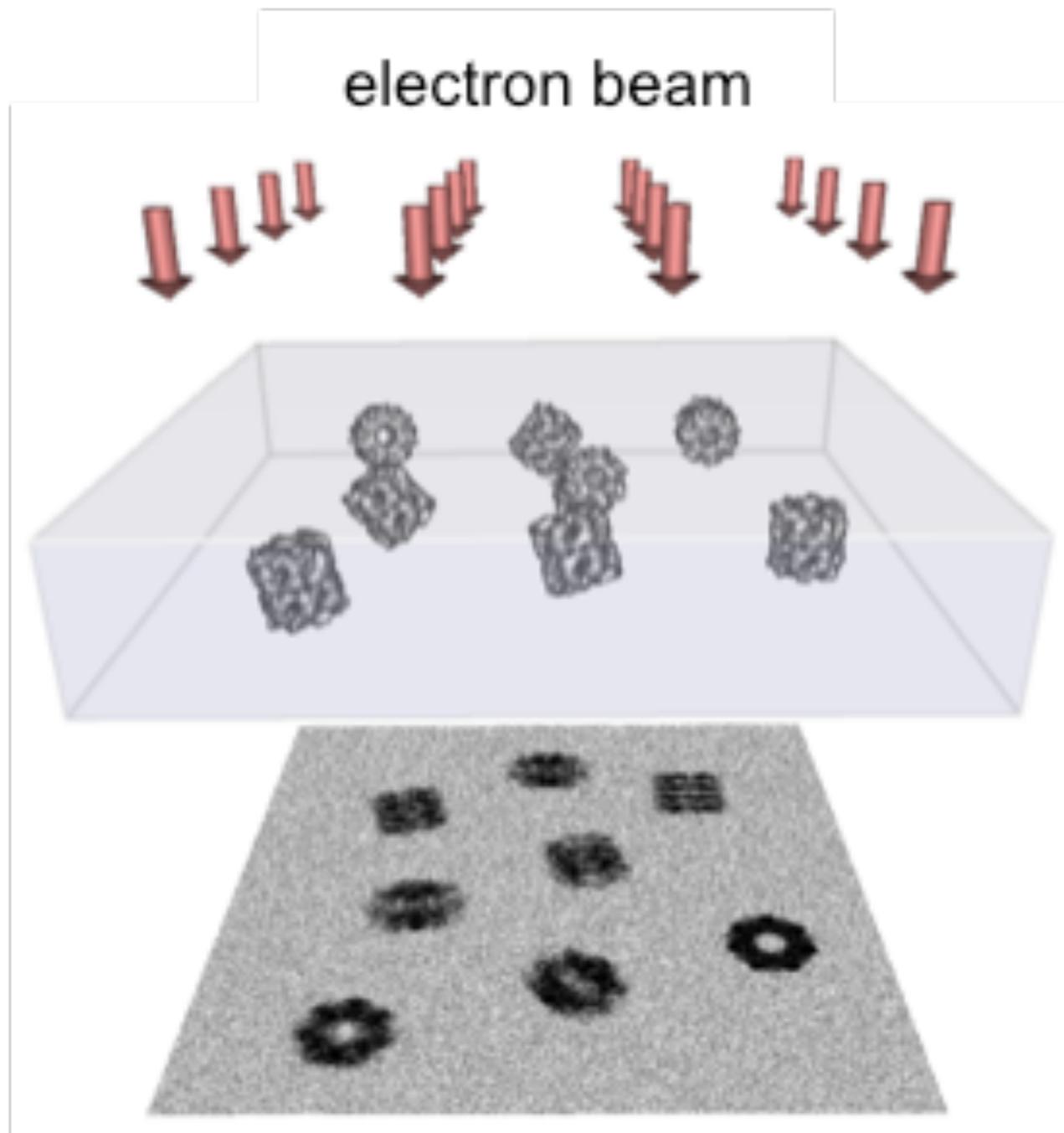


EM



X-ray

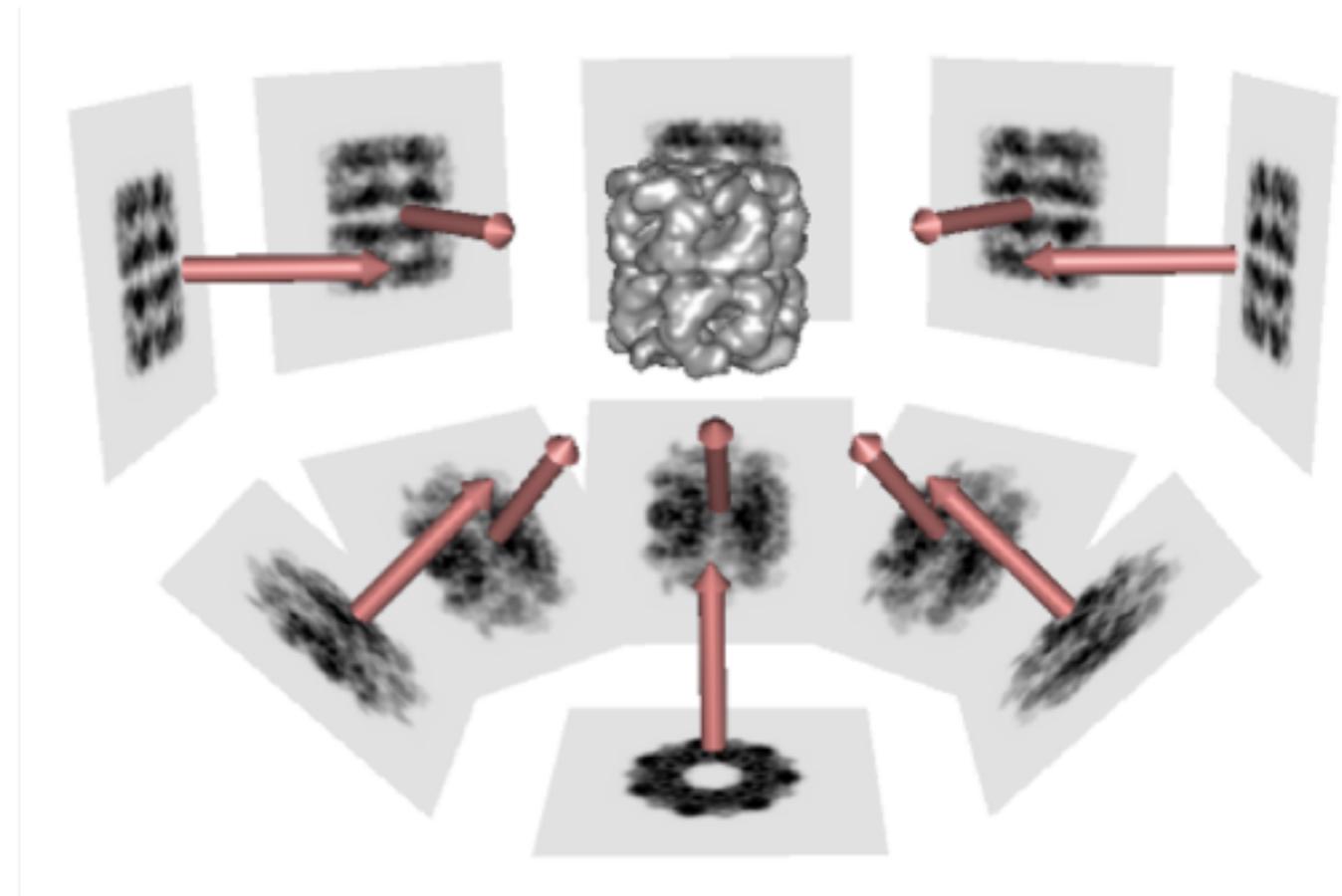
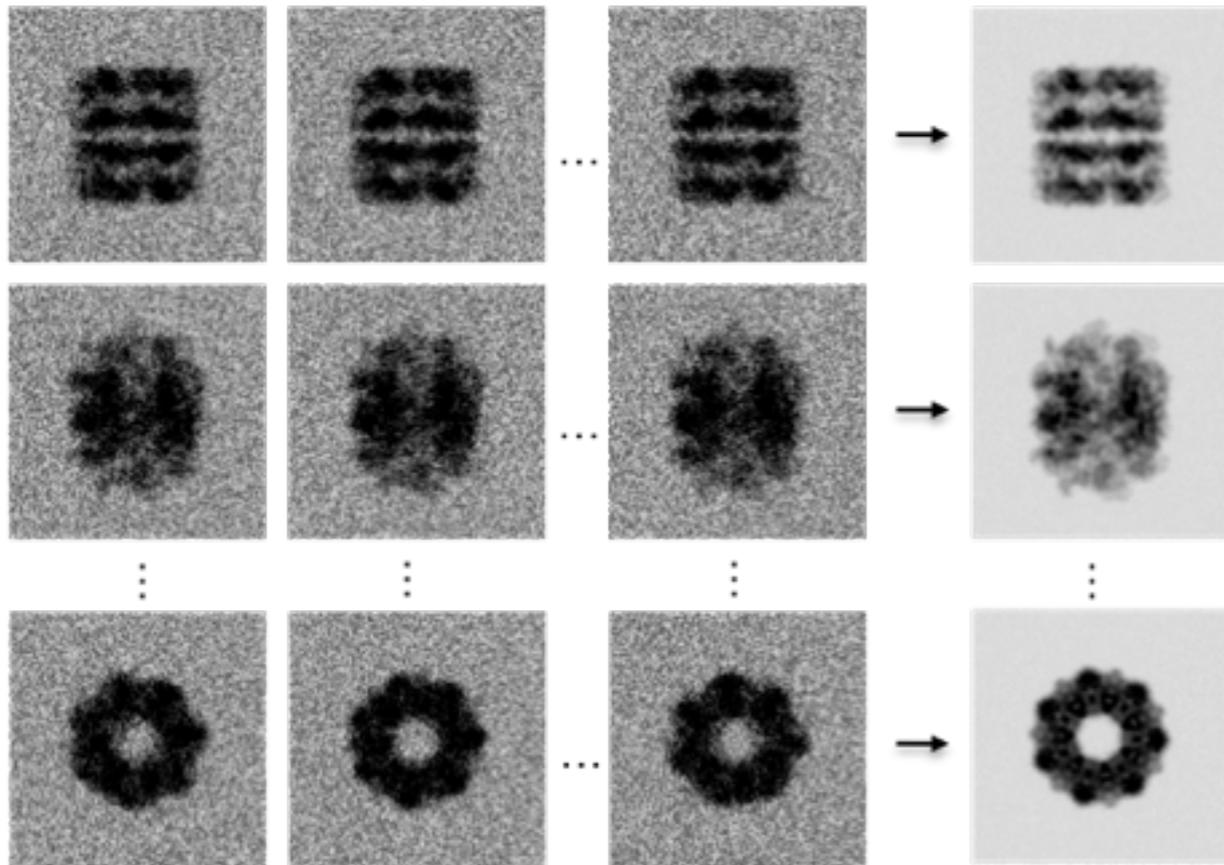
sorting the data



<http://people.csail.mit.edu/gdp/cryoem.html>

2D images are aligned and sorted computationally into classes representing homogeneous particles and perspectives

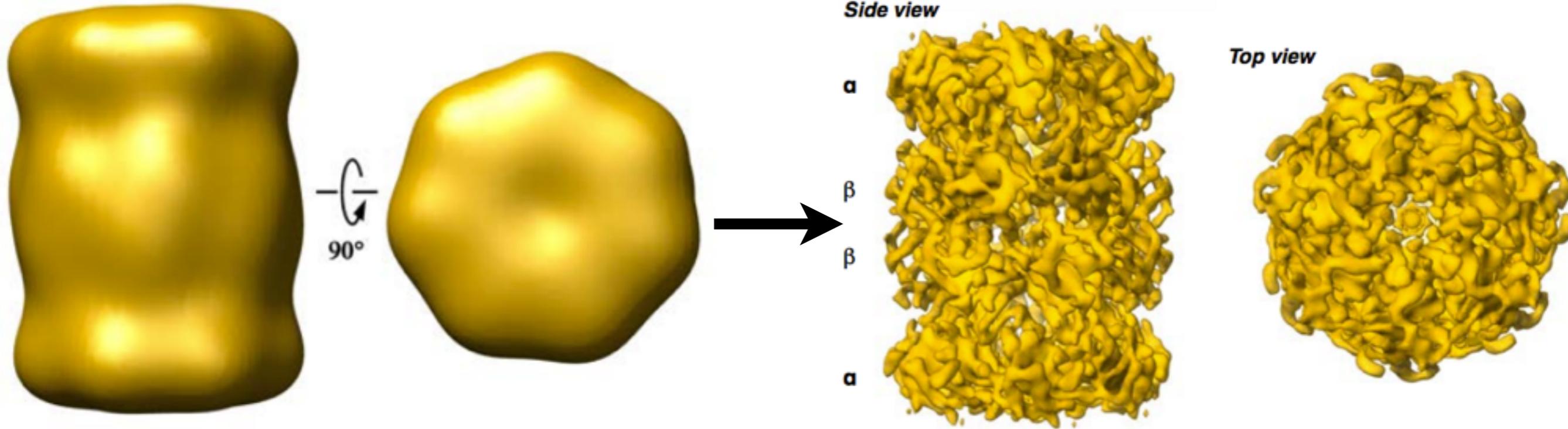
Class averages



<http://people.csail.mit.edu/gdp/cryoem.html>

classes are then averaged and back-projected to produce 3D density map

iterative refinement

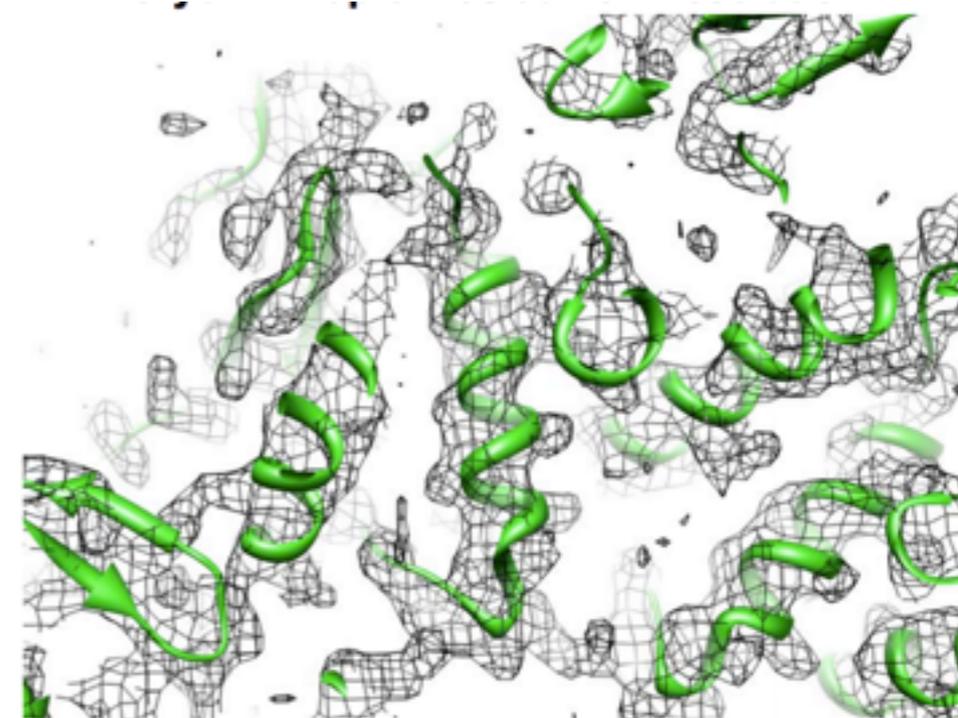


*cryo-EM map of the proteasome
(iteration 1)*

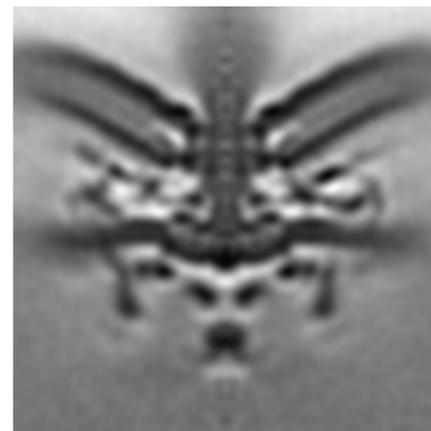
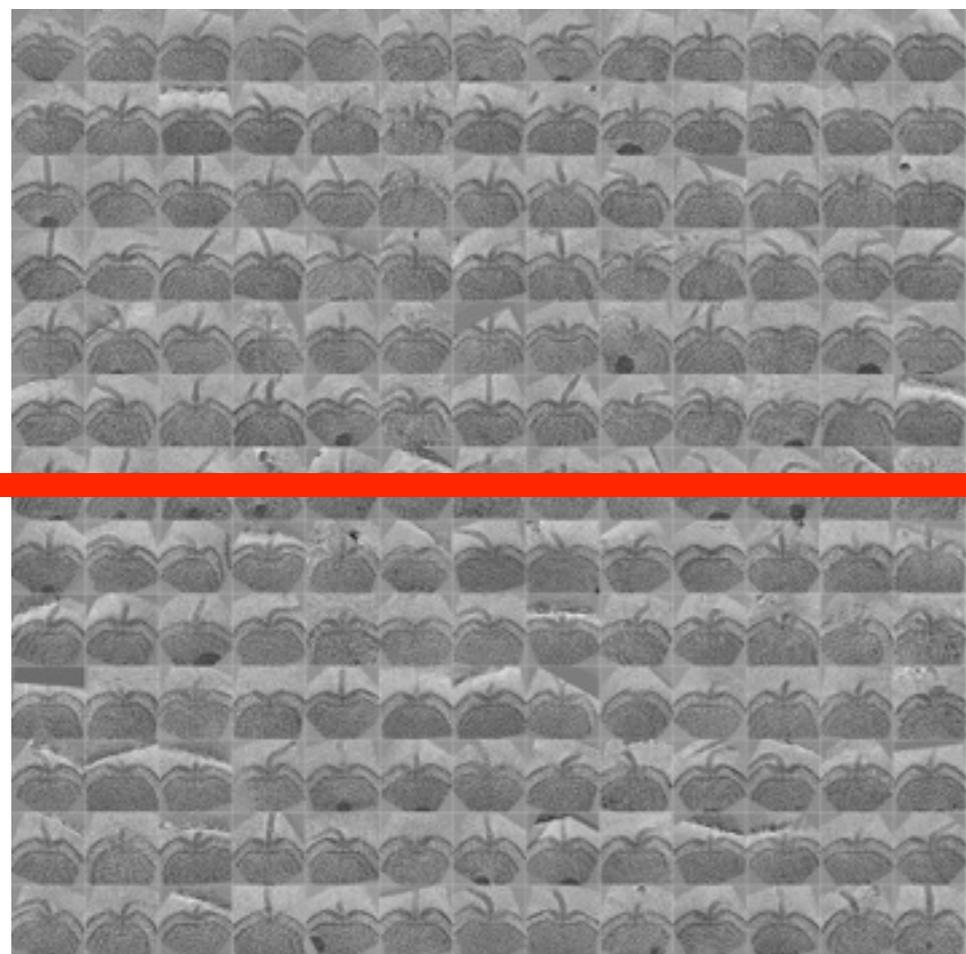
final map

back projection is iterative - need the model for
projection matching with class averages

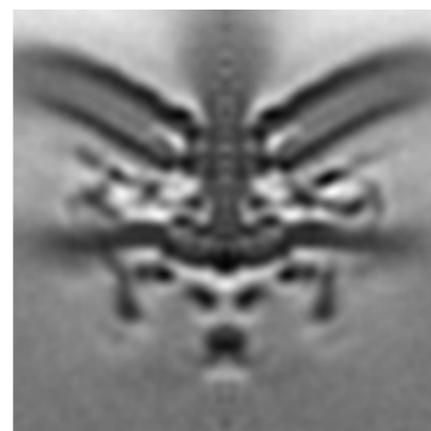
maps can have resolutions ranging from near-
atomic ($<5 \text{ \AA}$) to 2-3 nm



map resolution



Split dataset in half,
calculate two
independent
reconstructions

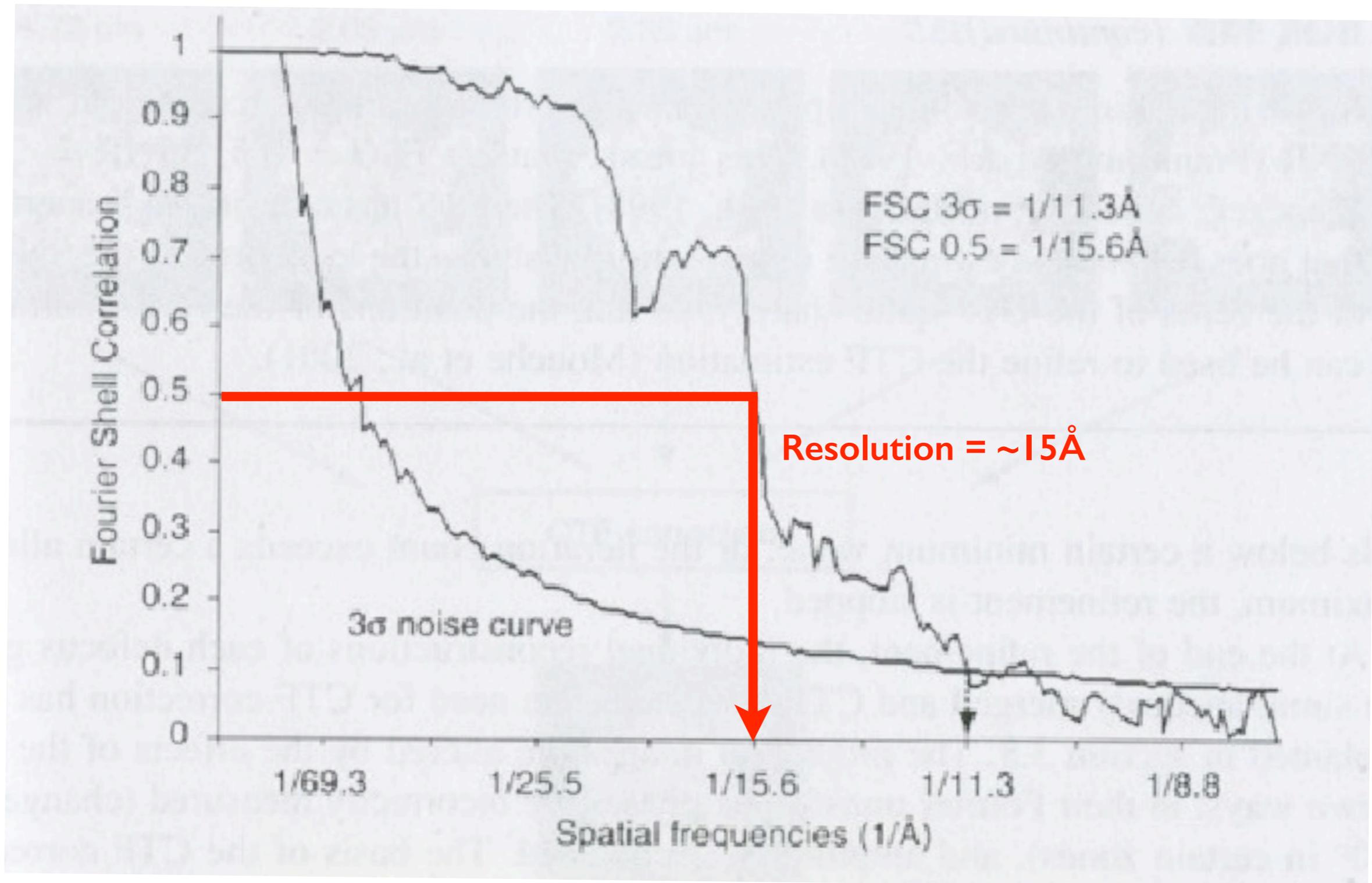


Align two
structures, flip
into reciprocal
space (i.e., 3D FT),
and calculate
correlation co-
efficients between
bands of spatial
frequency

Fourier shell correlation: $FSC(r) = \frac{\sum_{r_i \in r} F_1(r_i) \cdot F_2(r_i)^*}{\sqrt{\sum_{r_i \in r} |F_1(r_i)|^2 \cdot \sum_{r_i \in r} |F_2(r_i)|^2}}$

map resolution

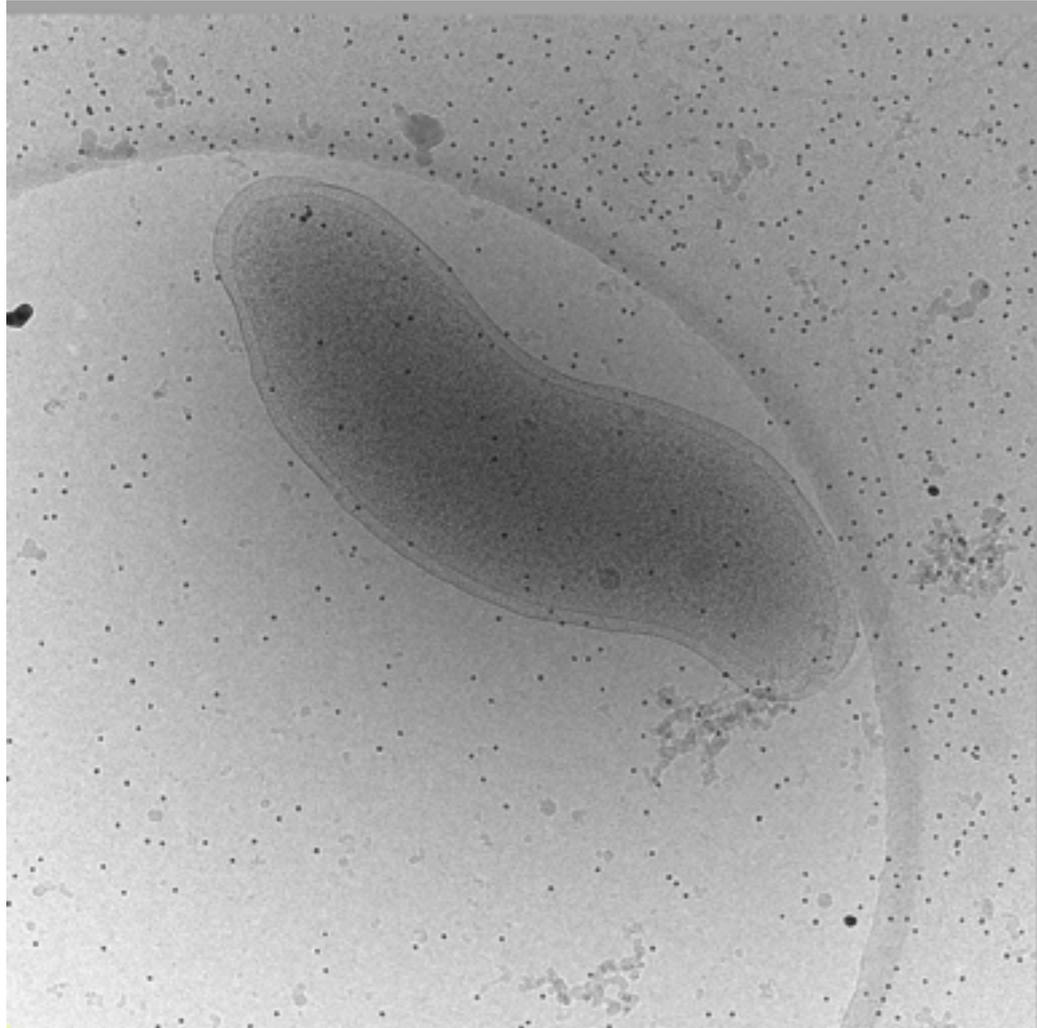
FSC between two halves of the data set



Electron cryo-tomography

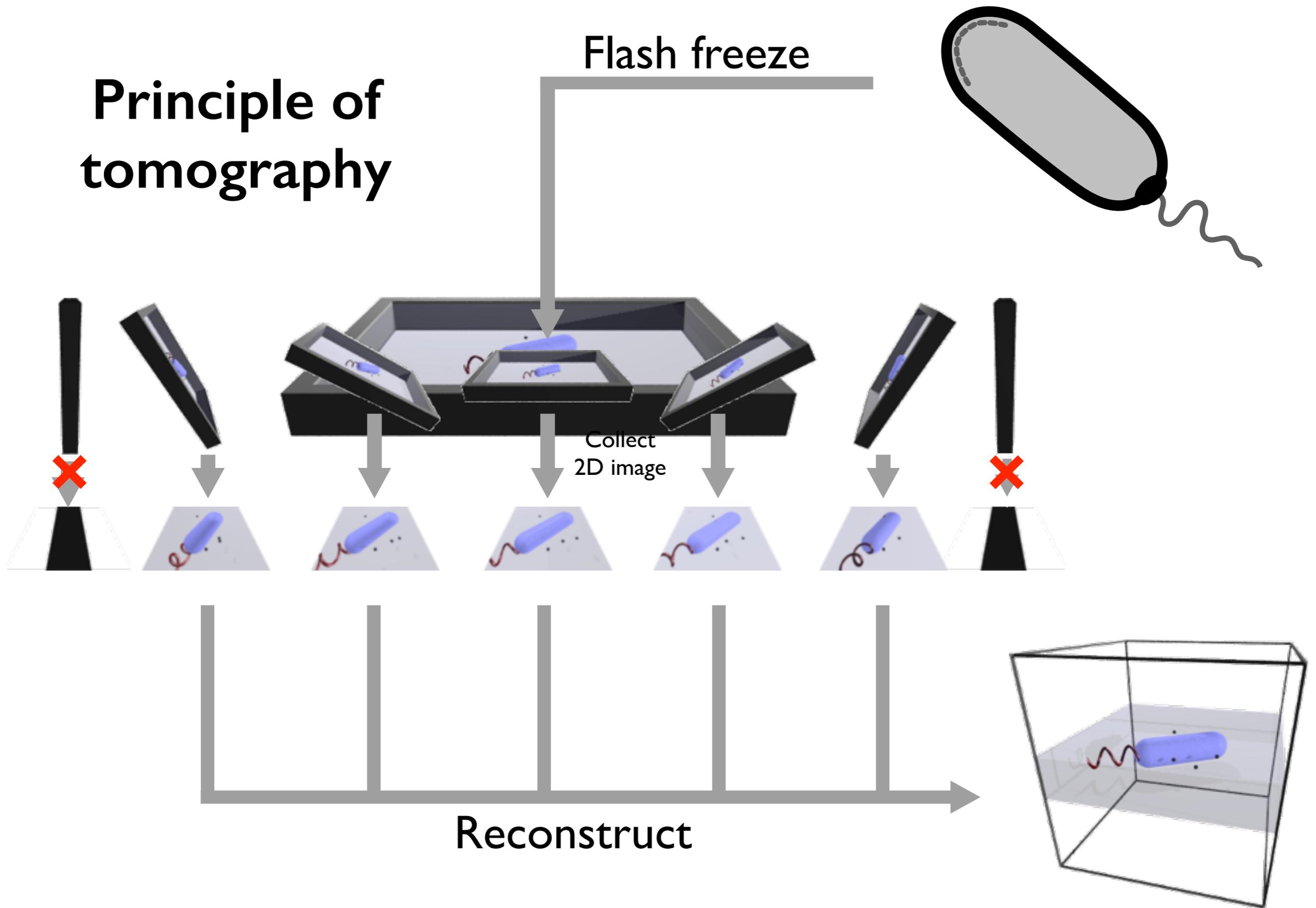
~100 2D images

3D tomogram



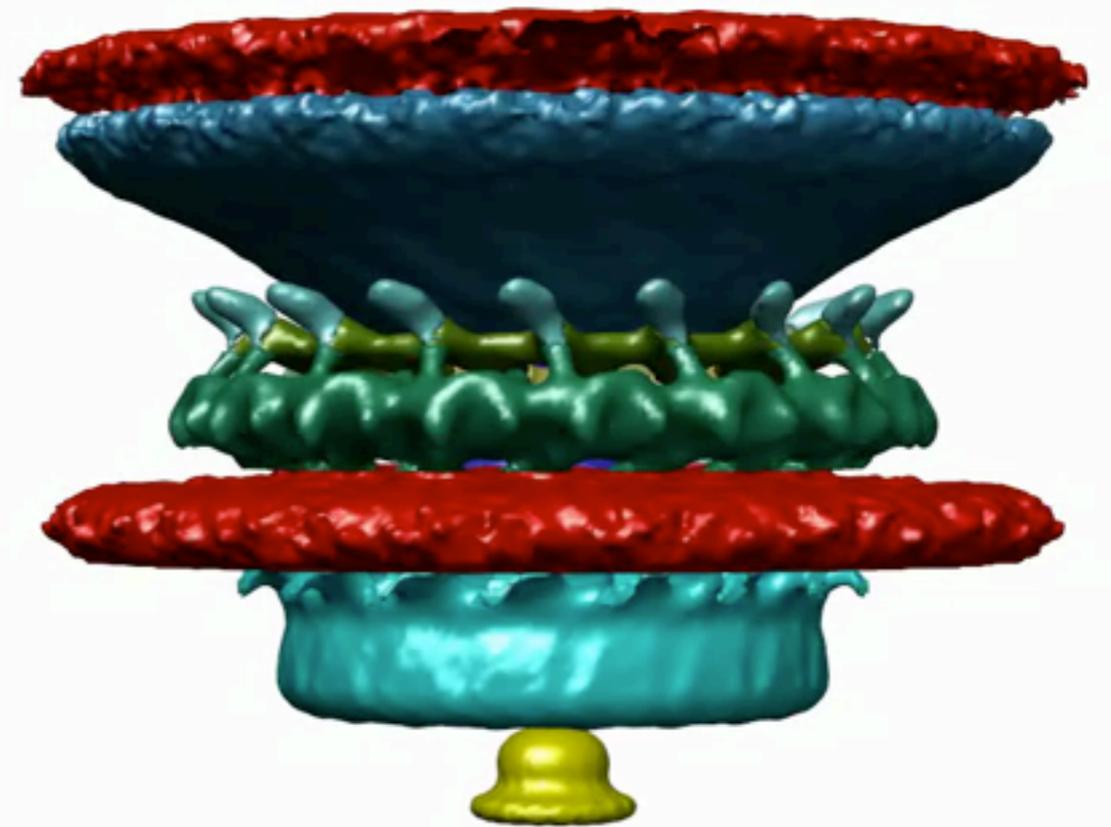
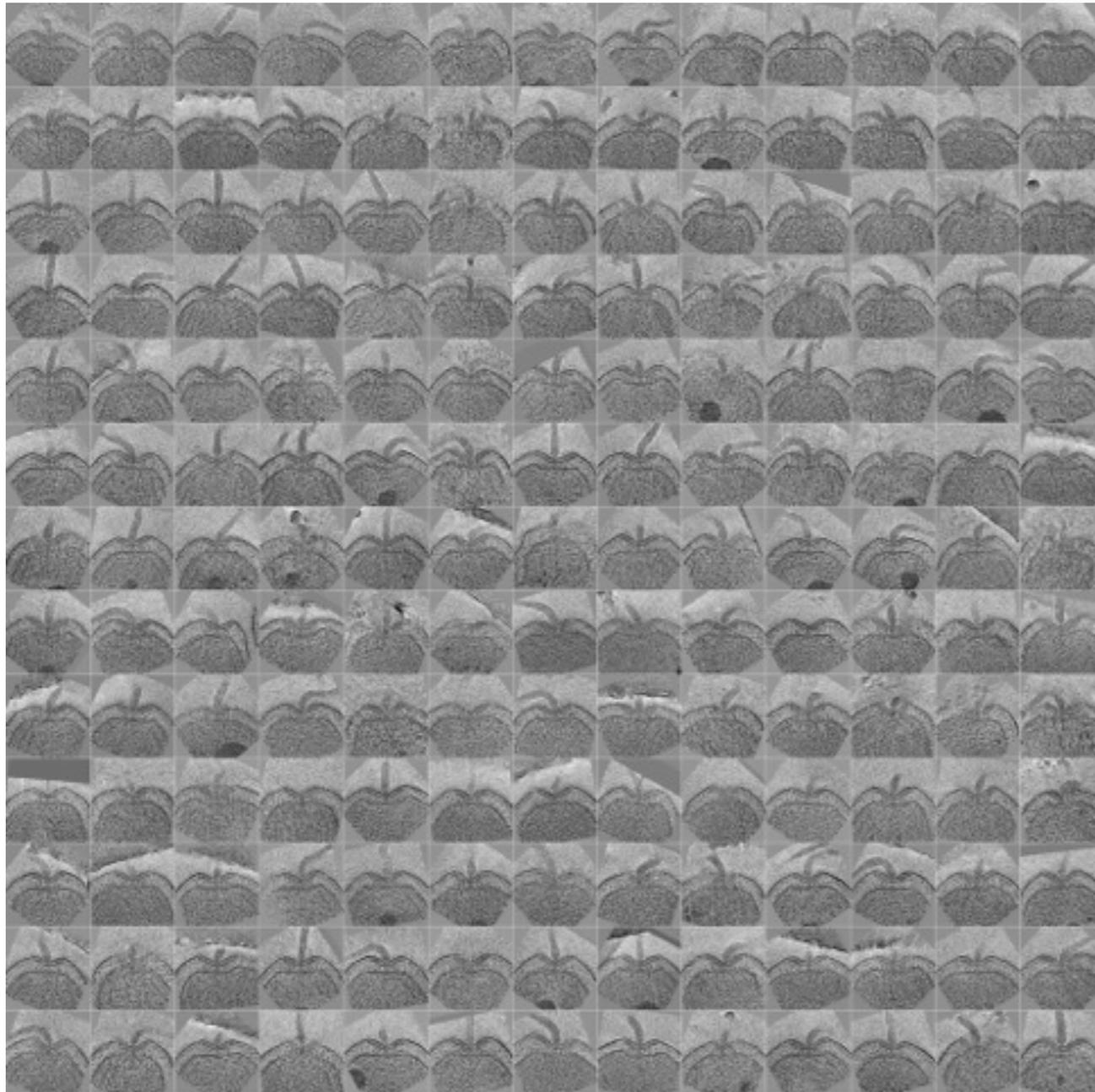
Reconstruct

Principle of tomography

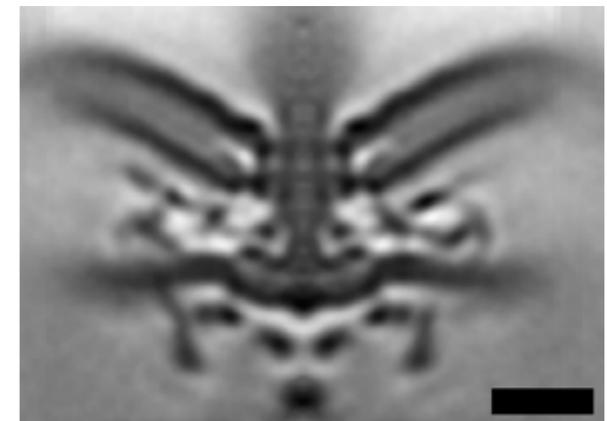


Subtomogram averaging

100's of ("identical") 3-D particles



Align and average



Identifying cellular features

